

Regularizing inverse problems using sparsity-based signal models



Jeffrey A. Fessler

William L. Root Professor of EECS

EECS Dept., BME Dept., Dept. of Radiology
University of Michigan

<http://web.eecs.umich.edu/~fessler>

Work with Sai Ravishankar and Raj Nadakuditi

CSP Seminar

31 Mar. 2016

- Research support from GE Healthcare
- Supported in part by NIH grants P01 CA-87634, U01 EB018753
- Equipment support from Intel Corporation

Why

- Low-dose X-ray CT imaging
- Accelerated MR imaging
- Other inverse problems

How

- MAP estimation for inverse problems
- Classical regularization methods (some sparsity based)
- Contemporary regularization methods (all sparsity based)

Why

- Low-dose X-ray CT imaging
- Accelerated MR imaging
- Other inverse problems

How

- MAP estimation for inverse problems
- Classical regularization methods (some sparsity based)
- Contemporary regularization methods (all sparsity based)

- A picture is worth 1000 words
- (and perhaps several 1000 seconds of computation?)



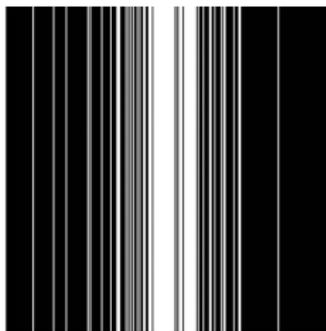
Thin-slice FBP
Seconds

ASIR (denoise)
A bit longer

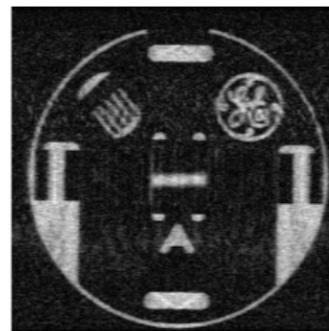
Statistical
Much longer

Today's talk: less about computation, more about image quality

Right image used **edge-preserving regularization**



(a)



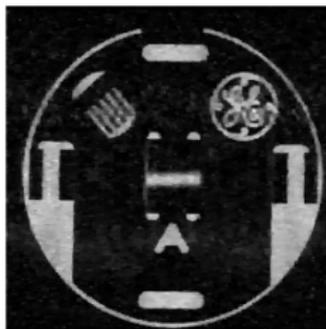
(b)

(a) $4\times$ under-sampled MR k-space

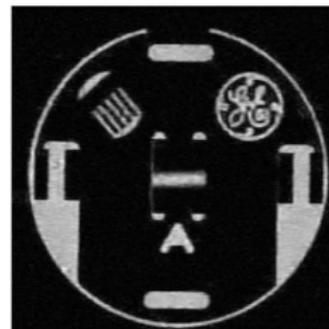
(b) zero-filled reconstruction

(c) “compressed sensing” reconstruction with TV regularization

(d) **adaptive dictionary learning regularization** [1, Fig. 10]



(c)



(d)

$$\mathbf{y} = \mathbf{A}\mathbf{x} + \boldsymbol{\varepsilon}$$

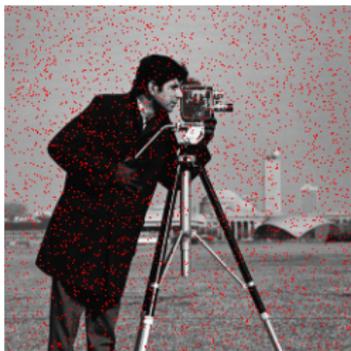
- ▶ compressed sensing
- ▶ deblurring (restoration)
- ▶ in-painting
- ▶ denoising (not ill posed)

(\mathbf{A} random, wide)

(\mathbf{A} Toeplitz, wide?)

(\mathbf{A} subset of rows of \mathbf{I})

($\mathbf{A} = \mathbf{I}$)



Why

- Low-dose X-ray CT imaging
- Accelerated MR imaging
- Other inverse problems

How

- MAP estimation for inverse problems
- Classical regularization methods (some sparsity based)
- Contemporary regularization methods (all sparsity based)

Why

- Low-dose X-ray CT imaging
- Accelerated MR imaging
- Other inverse problems

How

- MAP estimation for inverse problems**
- Classical regularization methods (some sparsity based)
- Contemporary regularization methods (all sparsity based)



If we have a prior $p(\mathbf{x})$, then the MAP estimate is:

$$\hat{\mathbf{x}} = \arg \max_{\mathbf{x}} p(\mathbf{x} | \mathbf{y}) = \arg \max_{\mathbf{x}} \log p(\mathbf{y} | \mathbf{x}) + \log p(\mathbf{x}).$$

For gaussian measurement errors and linear model:

$$-\log p(\mathbf{y} | \mathbf{x}) \equiv \frac{1}{2} \|\mathbf{y} - \mathbf{Ax}\|_{\mathbf{W}}^2$$

where $\|\mathbf{y}\|_{\mathbf{W}}^2 = \mathbf{y}'\mathbf{W}\mathbf{y}$

and $\mathbf{W}^{-1} = \text{Cov}\{\mathbf{y} | \mathbf{x}\}$ is known
(\mathbf{A} from physics, \mathbf{W} from statistics)

- ▶ If all images \mathbf{x} are “plausible” (have non-zero probability) then

$$p(\mathbf{x}) \propto e^{-R(\mathbf{x})} \implies -\log p(\mathbf{x}) \equiv R(\mathbf{x})$$

(from fantasy / imagination / wishful thinking)

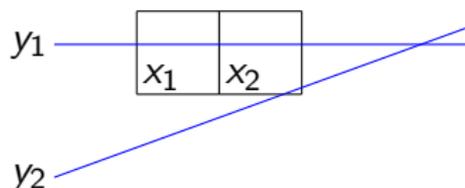
- ▶ MAP \equiv regularized weighted least-squares (WLS) estimation:

$$\begin{aligned}\hat{\mathbf{x}} &= \arg \max_{\mathbf{x}} \log p(\mathbf{y} | \mathbf{x}) + \log p(\mathbf{x}) \\ &= \arg \min_{\mathbf{x}} \frac{1}{2} \|\mathbf{y} - \mathbf{A}\mathbf{x}\|_{\mathbf{W}}^2 + R(\mathbf{x})\end{aligned}$$

- ▶ A regularizer $R(\mathbf{x})$, aka log prior, is essential for high-quality solutions to ill-conditioned / ill-posed inverse problems.
- ▶ Why ill-posed? High ambitions...

Example of ill-conditioned inverse problem

Two-pixel, two-ray “X-ray tomography” model:

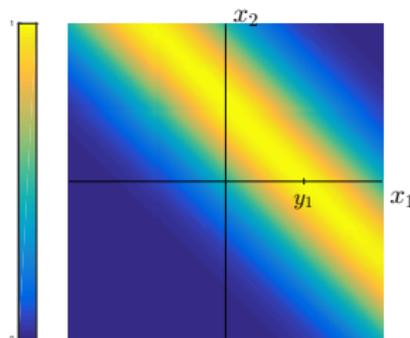


$$\mathbf{A} = \begin{bmatrix} 1 & 1 \\ 0 & 0.1 \end{bmatrix} \quad \mathbf{x} = \begin{bmatrix} x_1 \\ x_2 \end{bmatrix}$$

$\text{cond}(\mathbf{A}'\mathbf{A}) \approx 400$

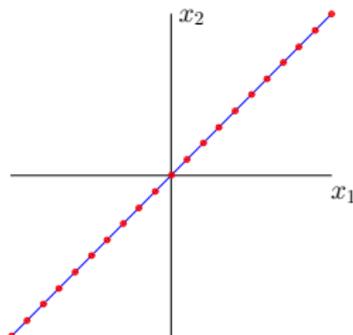
\mathbf{A} is (roughly) square - somewhat typical

log-likelihood $\log p(\mathbf{y}|\mathbf{x})$:



Subspace model: Alternative to regularization

Assuming \mathbf{x} lies in a sufficiently low-dimensional subspace could make an inverse problem well conditioned.



Assume $\mathbf{x} = \mathbf{D}\mathbf{z}$ where $\mathbf{D} = \begin{bmatrix} 1 \\ 1 \end{bmatrix}$ and $\mathbf{z} \in \mathbb{R}^1$

(\mathbf{z} has only one nonzero element so very sparse!?)

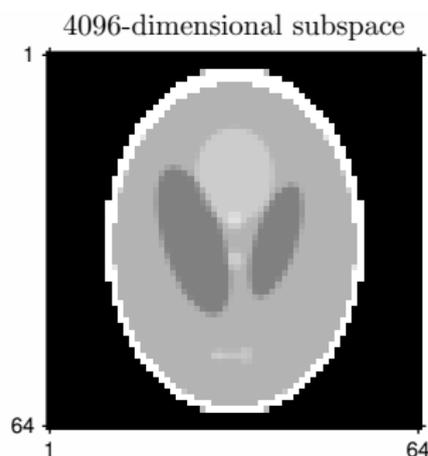
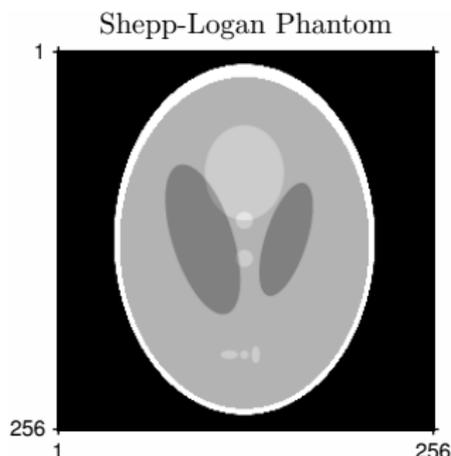
Estimate coefficient(s): $\hat{\mathbf{z}} = \arg \min_{\mathbf{z}} \|\mathbf{y} - \mathbf{A}\mathbf{D}\mathbf{z}\|_2^2$, then $\hat{\mathbf{x}} = \mathbf{D}\hat{\mathbf{z}}$,

where $\mathbf{B} \triangleq \mathbf{A}\mathbf{D} = \begin{bmatrix} 2 \\ 0.1 \end{bmatrix}$ and $\text{cond}(\mathbf{B}'\mathbf{B}) = 1$ which is perfect!

Why not use subspace models?

Candès and Romberg (2005) [2] used 22 (noiseless) projection views, each with 256 samples.

$22 \cdot 256 = 5632$ measured values, vs $256^2 = 65536$ unknown pixels



Subspace representation (using pixel basis) is undesirably coarse.

Why

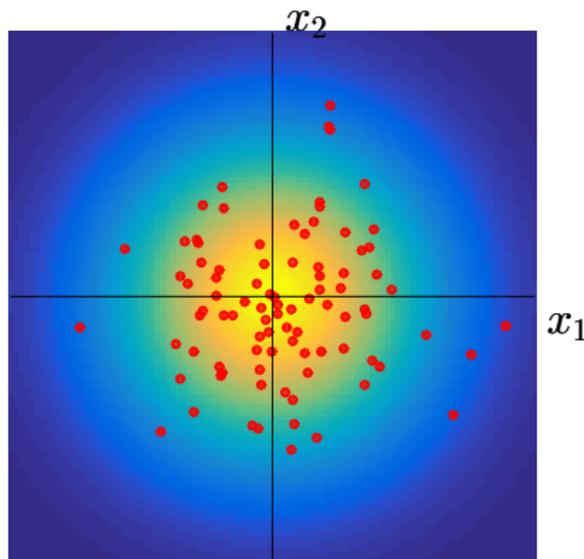
- Low-dose X-ray CT imaging
- Accelerated MR imaging
- Other inverse problems

How

- MAP estimation for inverse problems
- Classical regularization methods (some sparsity based)**
- Contemporary regularization methods (all sparsity based)

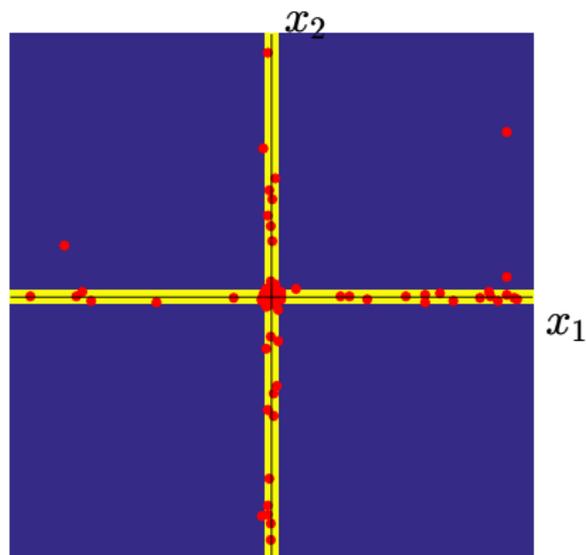
- ▶ Tikhonov regularization (IID gaussian prior)
- ▶ Roughness penalty (Basic MRF prior)
- ▶ Sparsity in ambient space
- ▶ Edge-preserving regularization
- ▶ Total-variation (TV) regularization
- ▶ Black-box denoiser like NLM

$$R(\mathbf{x}) = \beta \|\mathbf{x}\|_2^2$$



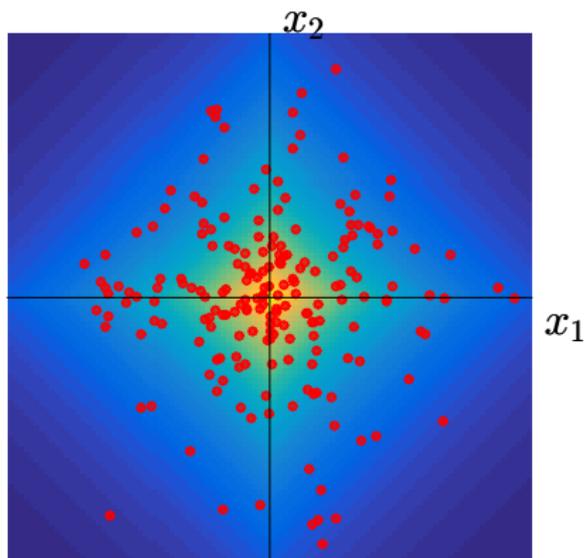
- ▶ Colors show equivalent (normalized) prior $p(\mathbf{x}) / p(\mathbf{0}) = e^{-R(\mathbf{x})}$
- ▶ Equivalent to IID gaussian prior on \mathbf{x}
- ▶ Makes any ill-conditioned / ill-posed problem well conditioned
- ▶ Ignores correlations between pixels

$$R(\mathbf{x}) = \beta \|\mathbf{x}\|_0 = \beta \sum_j \mathbb{I}_{\{x_j \neq 0\}}$$

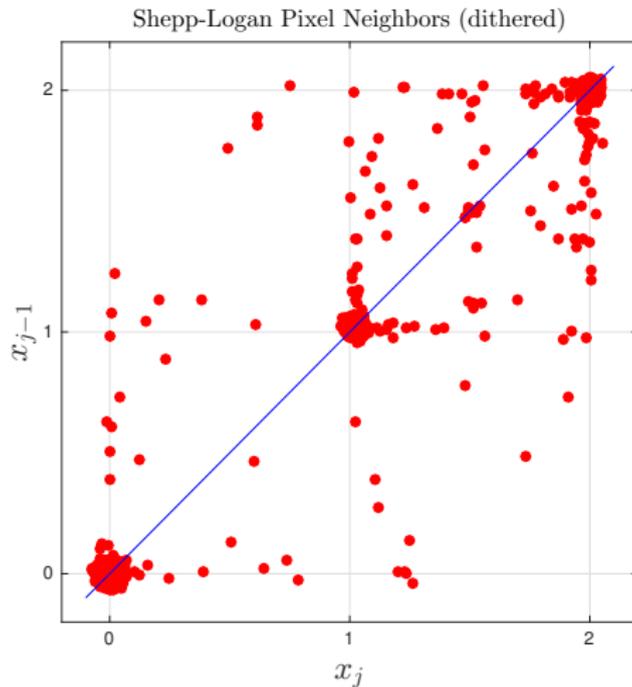
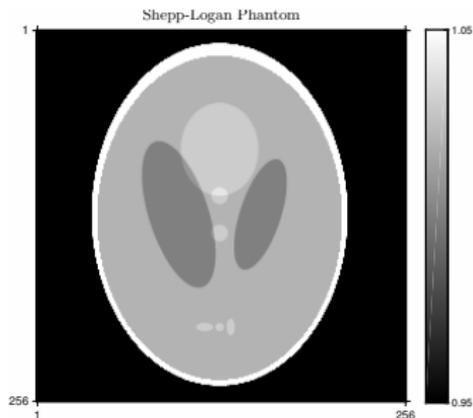


- ▶ Approximate Bayesian interpretation
- ▶ Non-convex
- ▶ IID \implies also ignores correlations

$$R(\mathbf{x}) = \beta \|\mathbf{x}\|_1 = \beta \sum_j |x_j|$$



- ▶ Equivalent to IID Laplacian prior on \mathbf{x}
- ▶ Also ignores correlations

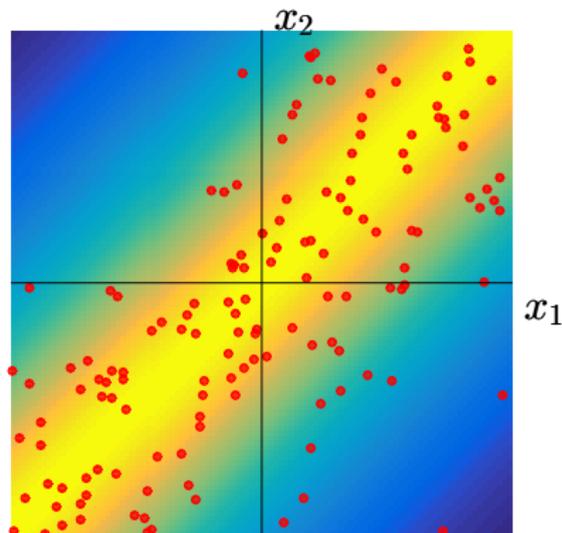
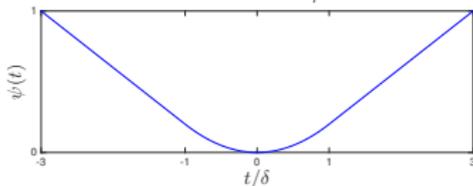


Caution: Shepp-Logan phantom [3] was designed for testing non-Bayesian methods, not for designing signal models. Q: What causes the spread??

Neighboring pixels tend to have similar values except near edges:

$$R(\mathbf{x}) = \beta \sum_j \psi(x_j - x_{j-1})$$

Potential function ψ :



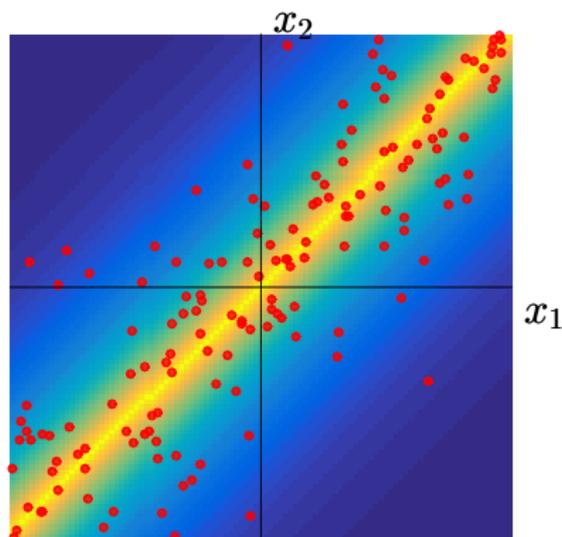
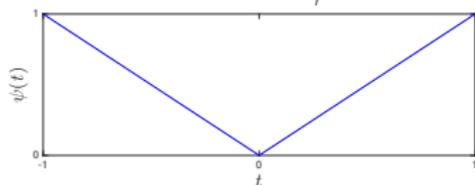
- Equivalent to improper prior (agnostic to DC value)
- Accounts for spatial correlations, but only very locally
- Used clinically now for low-dose X-ray CT image reconstruction

Total-variation (TV) regularization

Neighboring pixels tend to have similar values except near edges (“gradient sparsity”):

$$\begin{aligned} R(\mathbf{x}) &= \beta \text{TV}(\mathbf{x}) = \beta \|\mathbf{C}\mathbf{x}\|_1 \\ &= \beta \sum_j |x_j - x_{j-1}| \end{aligned}$$

Potential function ψ :



- ▶ Equivalent to improper prior (agnostic to DC value)
- ▶ Accounts for correlations, but only very locally
- ▶ Well-suited to piece-wise constant Shepp-Logan phantom!
- ▶ Used in many academic publications...

Noisy image \rightarrow Denoiser \rightarrow Denoised image

- ▶ Example: Non-local means (NLM)
- ▶ Corresponding regularizer [4]–[6]:

$$R(\mathbf{x}) = \beta \frac{1}{2} \|\mathbf{x} - \text{NLM}(\mathbf{x})\|_2^2$$

- ▶ Encourages self-consistency with denoised version of image
- ▶ No evident Bayesian interpretation
- ▶ Variable splitting can facilitate minimization [7].

- ▶ Transforms: wavelets, curvelets, ...
- ▶ Markov random field models
- ▶ Graphical models
- ▶ ...

Why

- Low-dose X-ray CT imaging
- Accelerated MR imaging
- Other inverse problems

How

- MAP estimation for inverse problems
- Classical regularization methods (some sparsity based)
- Contemporary regularization methods (all sparsity based)

- ▶ Convolutional sparsity
- ▶ Union of subspaces
- ▶ Sparse coding with dictionary
- ▶ manifolds? [8]

Idea:

$$\mathbf{x}[\vec{n}] \approx \sum_{k=1}^K h_k[\vec{n}] * z_k[\vec{n}]$$

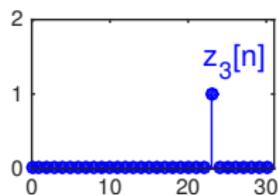
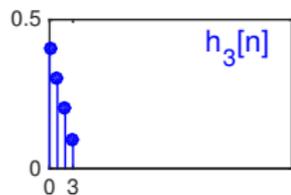
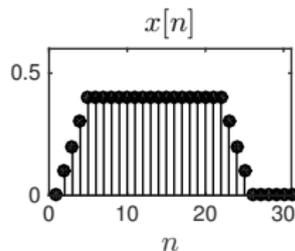
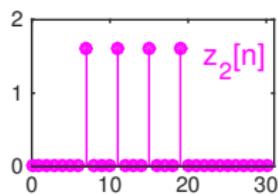
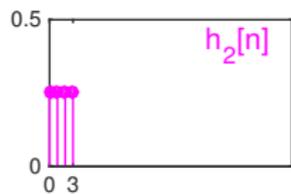
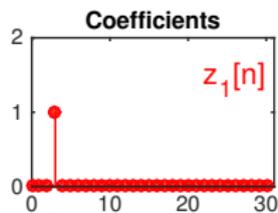
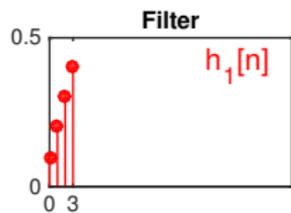
- where each $h_k[\vec{n}]$ is a FIR filter with $\|\mathbf{h}_k\| = 1$
- and each coefficient image $z_k[\vec{n}]$ is sparse [9]–[11].

Equivalent matrix-vector representation:

$$\mathbf{x} \approx \sum_{k=1}^K \mathbf{H}_k \mathbf{z}_k$$

where \mathbf{H}_k is a Toeplitz (or circulant) matrix corresponding to \mathbf{h}_k .

Convolutional sparsity: example



$$x[\vec{n}] \approx \sum_{k=1}^K h_k[\vec{n}] * z_k[\vec{n}]$$

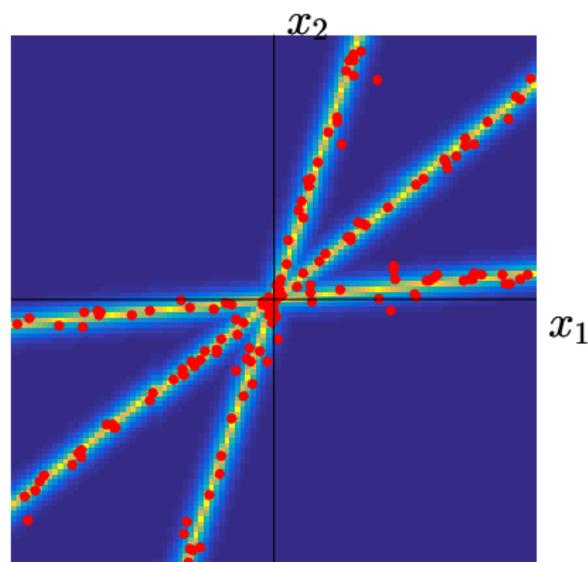
Recall $\mathbf{x} \approx \sum_{k=1}^K \mathbf{H}_k \mathbf{z}_k$

Natural corresponding regularizer:

$$R(\mathbf{x}) = \min_{\{\mathbf{z}_k\}} \min_{\substack{\{\mathbf{h}_k\} \\ \|\mathbf{h}_k\| = 1}} \left(\left\| \mathbf{x} - \sum_{k=1}^K \mathbf{H}_k \mathbf{z}_k \right\|_2^2 + \lambda^2 \sum_{k=1}^K \|\mathbf{z}_k\|_0 \right)$$

Adapts FIR filters $\{\mathbf{h}_k\}$ and coefficients $\{\mathbf{z}_k\}$ to candidate \mathbf{x} .

- Literature focuses on the minimization problem (sparse coding)
- Yet to be explored as regularizer for inverse problems
- Inherently shift-invariant representation; no “patches” needed



- ▶ Dimensionality reduction?
- ▶ *cf.* classification / clustering motivation [12]
- ▶ (Extension to union of “flats” (linear varieties) is possible [13].)

Given (?) collection of K subspace bases $\mathbf{D}_1, \dots, \mathbf{D}_K$
(dictionaries with full column rank):

$$\begin{aligned} R(\mathbf{x}) &= \underbrace{\min_k}_{\text{"classification"}} \underbrace{\min_{\mathbf{z}_k} \beta \frac{1}{2} \|\mathbf{x} - \mathbf{D}_k \mathbf{z}_k\|_2^2}_{\text{regression}} \\ &= \min_k \beta \frac{1}{2} \|\mathbf{x} - \mathbf{D}_k \mathbf{D}_k^+ \mathbf{x}\|_2^2 \end{aligned}$$

- ▶ $R(\mathbf{x}) = 0$ if \mathbf{x} lies in the span of any of the dictionaries $\{\mathbf{D}_k\}$.
- ▶ otherwise, distance to nearest subspace (discourage, not constrain)
- ▶ Non-convex (highly?) (cf. preceding picture)
- ▶ Apply to image patches to be practical
- ▶ Equivalent Bayesian interpretation? (not a mixture model here)

Assume $\mathbf{x} \approx \mathbf{D}\mathbf{z}$ where \mathbf{D} is a dictionary (often over-complete) and \mathbf{z} is a sparse coefficient vector. Corresponding regularizers:

$$R(\mathbf{x}) = \min_{\mathbf{z}: \|\mathbf{z}\|_p \leq s} \beta \frac{1}{2} \|\mathbf{x} - \mathbf{D}\mathbf{z}\|_2^2$$

$$R(\mathbf{x}) = \min_{\mathbf{z}} \left(\beta_1 \frac{1}{2} \|\mathbf{x} - \mathbf{D}\mathbf{z}\|_2^2 + \beta_2 \|\mathbf{z}\|_p \right)$$

- ▶ Convex in \mathbf{z} (for given \mathbf{x}) if $p \geq 1$.
- ▶ $R(\mathbf{x})$ typically non-convex in \mathbf{x} .
- ▶ Could be equivalent to a union-of-subspaces regularizer if $\mathbf{D} = [\mathbf{D}_1 \dots \mathbf{D}_K]$ and if we constrain coefficient vector \mathbf{z} in a non-standard way.

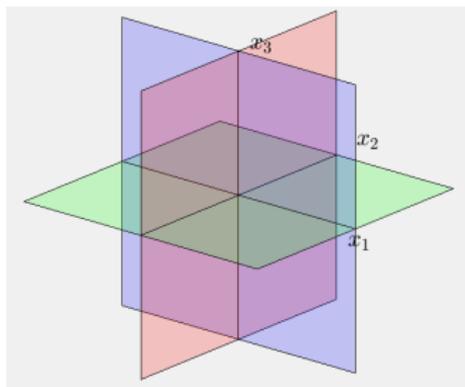
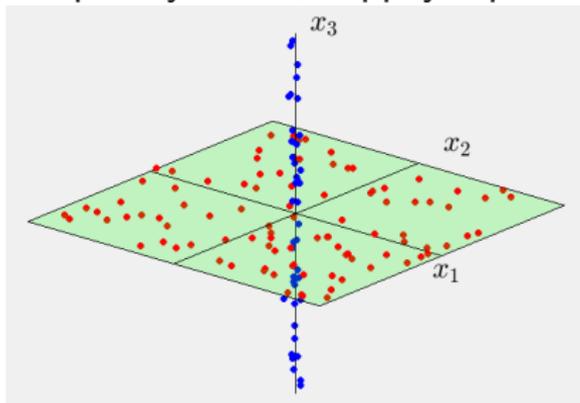
Union-of-subspaces vs sparse-coding-with-dictionary

Consider union-of-subspaces model with $\mathbf{D}_1 = \begin{bmatrix} 1 & 0 \\ 0 & 1 \\ 0 & 0 \end{bmatrix}$, $\mathbf{D}_2 = \begin{bmatrix} 0 \\ 0 \\ 1 \end{bmatrix}$.

So \mathbf{D}_1 spans x-y plane and \mathbf{D}_2 spans z-axis.

A dictionary model with $\mathbf{D} = [\mathbf{D}_1 \ \mathbf{D}_2] = \begin{bmatrix} 1 & 0 & 0 \\ 0 & 1 & 0 \\ 0 & 0 & 1 \end{bmatrix}$

and sparsity $s = 2$, happily represents all three cardinal planes



Thus dictionary model seems “less constrained” than union-of-subspaces model.

(Still, focus on sparse dictionary representation hereafter.)

Dictionary learning from training data

- Given training data $\mathbf{x}_1, \dots, \mathbf{x}_N \in \mathbb{R}^d$ (image patches)
- Assumed model: $\mathbf{x}_n \approx \mathbf{D}\mathbf{z}_n$
- unknown $d \times J$ dictionary $\mathbf{D} = [\mathbf{d}_1 \dots \mathbf{d}_J]$
- coefficient vectors $\mathbf{z}_1, \dots, \mathbf{z}_N \in \mathbb{R}^J$ assumed “sparse”

K-SVD dictionary learning formulation [14]:

$$\begin{aligned} \mathbf{D}^* &= \arg \min_{\mathbf{D} \in \mathbb{R}^{d \times J}} \sum_{n=1}^N \min_{\mathbf{z}_n \in \mathbb{R}^J} \|\mathbf{x}_n - \mathbf{D}\mathbf{z}_n\|_2 \quad \text{s.t.} \quad \begin{aligned} \|\mathbf{d}_j\| &= 1 \quad \forall j \\ \|\mathbf{z}_n\|_0 &\leq s \quad \forall n \end{aligned} \\ &= \arg \min_{\mathbf{D} \in \mathbb{R}^{d \times J}} \min_{\mathbf{Z} \in \mathbb{R}^{J \times N}} \|\mathbf{X} - \mathbf{D}\mathbf{Z}\|_F \quad \text{s.t.} \quad \begin{aligned} \|\mathbf{d}_j\| &= 1 \quad \forall j \\ \|\mathbf{z}_n\|_0 &\leq s \quad \forall n \end{aligned} \end{aligned}$$

$$\mathbf{X} \triangleq [\mathbf{x}_1 \dots \mathbf{x}_N], \quad \mathbf{Z} \triangleq [\mathbf{z}_1 \dots \mathbf{z}_N]$$

Computationally expensive and no convergence guarantees.

Inherently non-convex due to product of unknowns $\mathbf{D}\mathbf{Z}$.

New dictionary learning method (SOUP-DIL)

Joint work with Sai Ravishankar and Raj Nadakuditi [15]–[18]

- Write sparse representation as Sum of Outer Products (SOUP):

$$\mathbf{X} \approx \mathbf{DZ} = \mathbf{DC}' = \sum_{j=1}^J \mathbf{d}_j \mathbf{c}_j'$$

where $\mathbf{Z}' = \mathbf{C} = [\mathbf{c}_1 \ \dots \ \mathbf{c}_J] \in \mathbb{R}^{N \times J}$ (coefficients for each atom)

- Replace individual atom sparsity constraint $\|\mathbf{z}_n\|_0 \leq s$ with aggregate sparsity regularizer: $\|\mathbf{Z}\|_0 = \|\mathbf{C}\|_0$.
 - ▶ Natural for Dictionary Learning (DIL) from training data
 - ▶ Unnatural for image compression using sparse coding

SOUP-DIL ℓ_0 formulation:

$$\mathbf{D}^* = \arg \min_{\mathbf{D} \in \mathbb{R}^{d \times J}} \min_{\mathbf{C} \in \mathbb{R}^{N \times J}} \|\mathbf{X} - \mathbf{DC}'\|_F^2 + \lambda^2 \|\mathbf{C}\|_0 \quad \text{s.t.} \quad \begin{cases} \|\mathbf{d}_j\|_2 = 1 \quad \forall j \\ \|\mathbf{c}_j\|_\infty \leq L \quad \forall j \end{cases}$$

SOUP-DIL formulation:

$$\mathbf{D}^* = \arg \min_{\mathbf{D} \in \mathbb{R}^{d \times J}} \min_{\mathbf{C} \in \mathbb{R}^{N \times J}} \|\mathbf{X} - \mathbf{D}\mathbf{C}'\|_F^2 + \lambda^2 \|\mathbf{C}\|_0 \quad \text{s.t.} \quad \begin{aligned} \|\mathbf{d}_j\|_2 &= 1 \quad \forall j \\ \|\mathbf{c}_j\|_\infty &\leq L \quad \forall j \end{aligned}$$

- ▶ Block coordinate descent (BCD) algorithm
 - Sparse coding step for \mathbf{C}
 - Dictionary update step for \mathbf{D}
- ▶ Very simple update rules (low compute cost)
- ▶ Monotone descent of $\Psi(\mathbf{D}, \mathbf{C})$
- ▶ Convergence theorem: for any given initialization $(\mathbf{D}^0, \mathbf{C}^0)$, all accumulation points of sequence (\mathbf{D}, \mathbf{C})
 - are critical points of cost Ψ and
 - are equivalent (reach same cost function value Ψ^*).
 - Furthermore: $\left\{ \|\mathbf{D}^{(k)} - \mathbf{D}^{(k-1)}\| \right\} \rightarrow 0$. Same for $\left\{ \mathbf{C}^{(k)} \right\}$.

$$\mathbf{D}^* = \arg \min_{\mathbf{D} \in \mathbb{R}^{d \times J}} \min_{\mathbf{C} \in \mathbb{R}^{N \times J}} \|\mathbf{X} - \mathbf{DC}'\|_F^2 + \lambda^2 \|\mathbf{C}\|_0 \quad \text{s.t.} \quad \begin{aligned} \|\mathbf{d}_j\|_2 &= 1 \quad \forall j \\ \|\mathbf{c}_j\|_\infty &\leq L \quad \forall j \end{aligned}$$

Alternate: update one column \mathbf{d}_j of \mathbf{D} then one column \mathbf{c}_j of \mathbf{C} .

- ▶ Sparse coding step: update \mathbf{c}_j using residual $\mathbf{E}_j \triangleq \sum_{k \neq j} \mathbf{d}_k \mathbf{c}'_k$

$$\min_{\mathbf{c}_j} \|\mathbf{E}_j - \mathbf{d}_j \mathbf{c}'_j\|_F^2 + \lambda^2 \|\mathbf{c}_j\|_0 \quad \text{s.t.} \quad \|\mathbf{c}_j\|_\infty \leq L$$

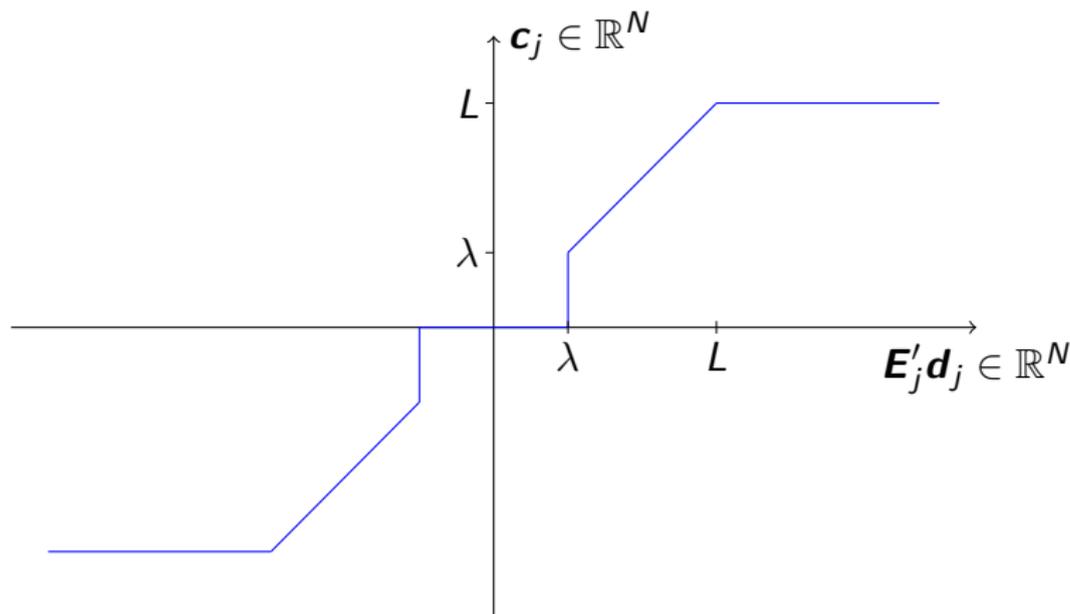
Truncated (via L) hard thresholding of $\mathbf{E}'_j \mathbf{d}_j$ with threshold λ

- ▶ Dictionary atom step: update \mathbf{d}_j

$$\min_{\mathbf{d}_j} \|\mathbf{E}_j - \mathbf{d}_j \mathbf{c}'_j\|_F^2 \quad \text{s.t.} \quad \|\mathbf{d}_j\|_2 = 1$$

Constrained least-squares solution: $\mathbf{d}_j = (\mathbf{E}_j \mathbf{c}_j) / \|\mathbf{E}_j \mathbf{c}_j\|_2$

Truncated hard thresholding for SOUP-DIL



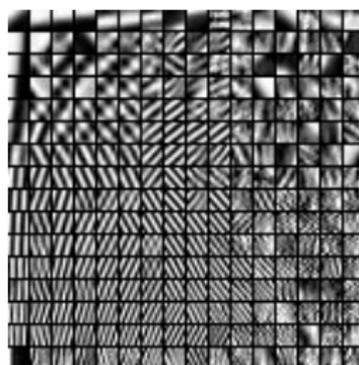
(Acts element-wise.) (In practice take $L = \infty$.)

(Algorithm also provides a simple sparse coding method.)

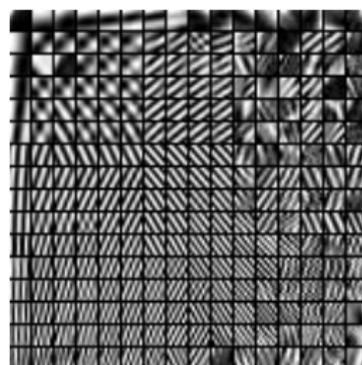
Example: dictionary learning for Barbara



Barbara



K-SVD D



SOUP-DIL D

Denosing PSNR (dB) from [15]

σ	Noisy	O-DCT	K-SVD	SOUP-DIL
20	22.13	29.95	30.83	30.79
25	20.17	28.68	29.63	29.64
30	18.59	27.62	28.54	28.63
100	8.11	21.87	21.87	21.97

SOUP-DIL faster than K-SVD

- ▶ Large image \mathbf{x} , extract M patches $\mathbf{X} = [\mathbf{P}_1\mathbf{x} \dots \mathbf{P}_M\mathbf{x}]$
- ▶ Assume patch $\mathbf{x}_m = \mathbf{P}_m\mathbf{x} \approx \mathbf{D}\mathbf{z}_m$ has (aggregate) sparse representation in dictionary $\mathbf{D} \in \mathbb{R}^{d \times J}$ where d is patch size

$$R(\mathbf{x}) = R(\mathbf{X}) = \min_{\mathbf{C} \in \mathbb{R}^{M \times J}} \|\mathbf{X} - \mathbf{D}\mathbf{C}'\|_F^2 + \lambda^2 \|\mathbf{C}\|_0 \quad \text{s.t.} \quad \|\mathbf{c}_j\|_\infty \leq L \quad \forall j$$

- ▶ $R(\mathbf{x}) = 0$ if patches can be represented exactly with “sufficiently few” non-zero coefficients (depends on λ)
- ▶ Ignore constraint $\|\mathbf{c}_j\|_\infty \leq L$
- ▶ Bayesian interpretation?

$$\begin{aligned}\hat{\mathbf{x}} &= \arg \min_{\mathbf{x}} \frac{1}{2} \|\mathbf{y} - \mathbf{A}\mathbf{x}\|_{\mathbf{W}}^2 + \beta R(\mathbf{x}) \\ &= \arg \min_{\mathbf{x}} \min_{\mathbf{C} \in \mathbb{R}^{M \times J}} \frac{1}{2} \|\mathbf{y} - \mathbf{A}\mathbf{x}\|_{\mathbf{W}}^2 + \frac{\beta}{2} \left(\|\mathbf{X} - \mathbf{D}\mathbf{C}'\|_{\mathbf{F}}^2 + \lambda^2 \|\mathbf{C}\|_0 \right)\end{aligned}$$

Alternating (nested) minimization:

- Fixing \mathbf{x} , updating each column of \mathbf{C} sequentially involves (truncated?) hard-thresholding
- Fixing \mathbf{C} , updating \mathbf{x} is (large-scale) quadratic problem

$$g(\mathbf{x}) = \frac{1}{2} \|\mathbf{X} - \mathbf{D}\mathbf{C}'\|_{\mathbf{F}}^2 = \sum_{m=1}^M \frac{1}{2} \|\mathbf{P}_m \mathbf{x} - \mathbf{D}\mathbf{P}_m \mathbf{C}'\|_2^2$$

$$\nabla^2 g(\mathbf{x}) = \sum_{m=1}^M \mathbf{P}_m' \mathbf{P}_m \quad \text{is diagonal}$$

- Work in progress...

- ▶ Numerous “normal-dose” CT images!
- ▶ learn \mathbf{D} , or most of it, from “big data”
- ▶ learn statistics of sparse coefficients \mathbf{Z} ?
- ▶ replace generic $\|\mathbf{Z}\|_0$ with $p(\mathbf{Z})$?

- ▶ Use majorization to update multiple columns of D or C simultaneously
- ▶ DC atom
- ▶ Rotate/flip atoms [19] [20]
- ▶ rank constraints on dictionary atoms [16]
- ▶ Tensor structured atoms for 3D / dynamic imaging
- ▶ Combined transform learning / dictionary learning
- ▶ Union of manifolds instead of union of subspaces?
- ▶ ...

Open problems

- Model selection
- Parameter selection
- Performance guarantees

- [1] S. Ravishanker and Y. Bresler, "MR image reconstruction from highly undersampled k-space data by dictionary learning," *IEEE Trans. Med. Imag.*, vol. 30, no. 5, 1028–41, May 2011.
- [2] E. Candès and J. K. Romberg, "Signal recovery from random projections," in *Proc. SPIE 5674 Computational Imaging III*, 2005, 76–86.
- [3] L. A. Shepp and B. F. Logan, "The Fourier reconstruction of a head section," *IEEE Trans. Nuc. Sci.*, vol. 21, no. 3, 21–43, Jun. 1974.
- [4] M. Mignotte, "A non-local regularization strategy for image deconvolution," *Pattern Recognition Letters*, vol. 29, no. 16, 2206–12, Dec. 2008.
- [5] Z. Yang and M. Jacob, "Nonlocal regularization of inverse problems: A unified variational framework," *IEEE Trans. Im. Proc.*, vol. 22, no. 8, 3192–203, Aug. 2013.
- [6] H. Zhang, J. Ma, J. Wang, Y. Liu, H. Lu, and Z. Liang, "Statistical image reconstruction for low-dose CT using nonlocal means-based regularization," *Computerized Medical Imaging and Graphics*, vol. 38, no. 6, 423–35, Sep. 2014.
- [7] S. Y. Chun, Y. K. Dewaraja, and J. A. Fessler, "Alternating direction method of multiplier for tomography with non-local regularizers," *IEEE Trans. Med. Imag.*, vol. 33, no. 10, 1960–8, Oct. 2014.
- [8] S. Poddar and M. Jacob, "Dynamic MRI using smoothness regularization on manifolds (SToRM)," *IEEE Trans. Med. Imag.*, 2016.
- [9] J. Yang, K. Yu, and T. Huang, "Supervised translation-invariant sparse coding," in *Proc. IEEE Conf. on Comp. Vision and Pattern Recognition*, 2010, 3517–24.
- [10] H. Bristow, A. Eriksson, and S. Lucey, "Fast convolutional sparse coding," in *Proc. IEEE Conf. on Comp. Vision and Pattern Recognition*, 2013, 391–8.
- [11] B. Wohlberg, "Efficient convolutional sparse coding," in *Proc. IEEE Conf. Acoust. Speech Sig. Proc.*, 2014, 7173–7.

- [12] R. Vidal, "Subspace clustering," *IEEE Sig. Proc. Mag.*, vol. 28, no. 2, 52–68, Mar. 2011.
- [13] T. Zhang, A. Szlam, and G. Lerman, "Median K-Flats for hybrid linear modeling with many outliers," in *Proc. Intl. Conf. Comp. Vision*, 2009, 234–41.
- [14] M. Aharon, M. Elad, and A. Bruckstein, "K-SVD: an algorithm for designing overcomplete dictionaries for sparse representation," *IEEE Trans. Sig. Proc.*, vol. 54, no. 11, 4311–22, Nov. 2006.
- [15] S. Ravishankar, R. R. Nadakuditi, and J. A. Fessler, "Efficient sum of outer products dictionary learning (SOUP-DIL) - The ℓ_0 method," *IEEE Trans. Sig. Proc.*, 2015, Submitted.
- [16] —, "Efficient learning of dictionaries with low-rank atoms," in *Proc. IEEE Intl. Conf. on Image Processing*, Submitted., 2016.
- [17] —, "Efficient l0 dictionary learning with convergence guarantees," in *Proc. Intl. Conf. Mach. Learn.*, Submitted., 2016.
- [18] —, *Efficient sum of outer products dictionary learning (SOUP-DIL) - The ℓ_0 method*, [arxiv 1511.08842](#), 2015.
- [19] B. Wen, S. Ravishankar, and Y. Bresler, *FRIST - flipping and rotation invariant sparsifying transform learning and applications of inverse problems*, 2016.
- [20] B. Wen, Y. Bresler, and S. Ravishankar, *FRIST - flipping and rotation invariant sparsifying transform learning and applications*, [arxiv 1511.06359](#), 2015.