

Part 4. Performance Characteristics

- Spatial resolution properties
- Noise properties
- Detection properties

Spatial Resolution Properties

Choosing β can be painful, so ...

For true minimization methods:

$$\hat{\boldsymbol{x}} = \arg \min_{\boldsymbol{x}} \Psi(\boldsymbol{x})$$

the *local impulse response* is approximately (Fessler and Rogers, T-MI, Sep. 1996):

$$l_j(\boldsymbol{x}) = \lim_{\delta \rightarrow 0} \frac{E[\hat{\boldsymbol{x}}|\boldsymbol{x} + \delta \boldsymbol{e}_j] - E[\hat{\boldsymbol{x}}|\boldsymbol{x}]}{\delta} \approx [-\nabla^{20}\Psi]^{-1} \nabla^{11}\Psi \frac{\partial}{\partial x_j} \bar{\boldsymbol{y}}(\boldsymbol{x}).$$

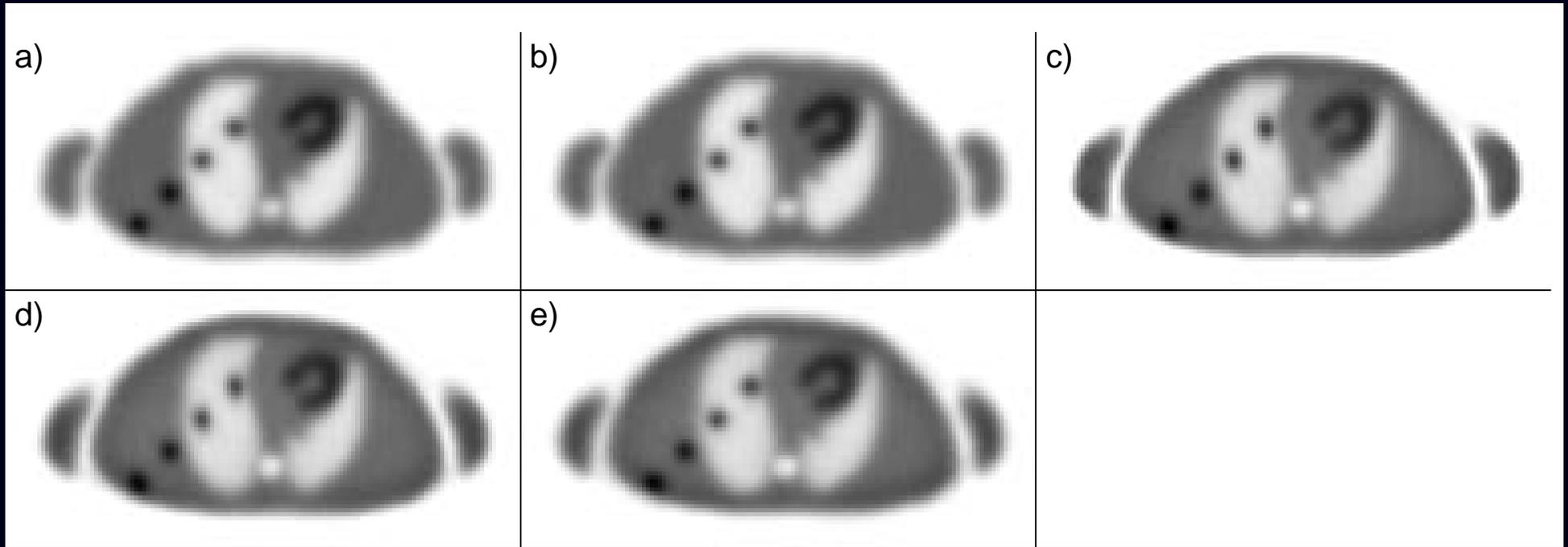
Depends only on chosen *cost function* and *statistical model*.
Independent of optimization algorithm.

- Enables prediction of resolution properties (provided Ψ is minimized)
- Useful for designing regularization penalty functions with desired resolution properties

$$l_j(\boldsymbol{x}) \approx [\boldsymbol{A}'\boldsymbol{W}\boldsymbol{A} + \beta\boldsymbol{R}]^{-1} \boldsymbol{A}'\boldsymbol{W}\boldsymbol{A}\boldsymbol{x}^{\text{true}}.$$

- Helps choose β for desired spatial resolution

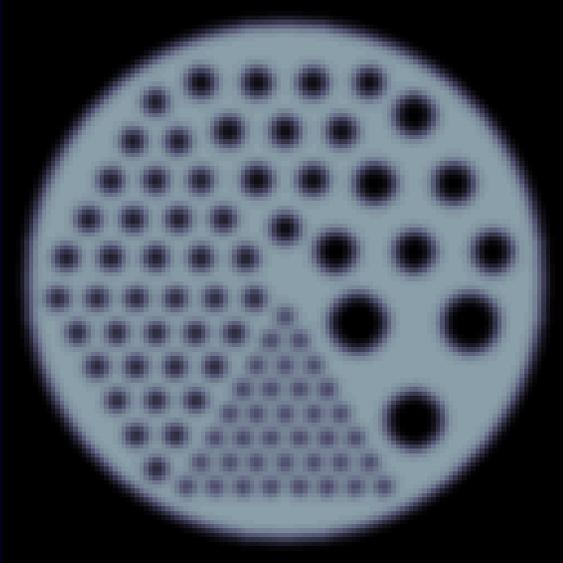
Modified Penalty Example, PET



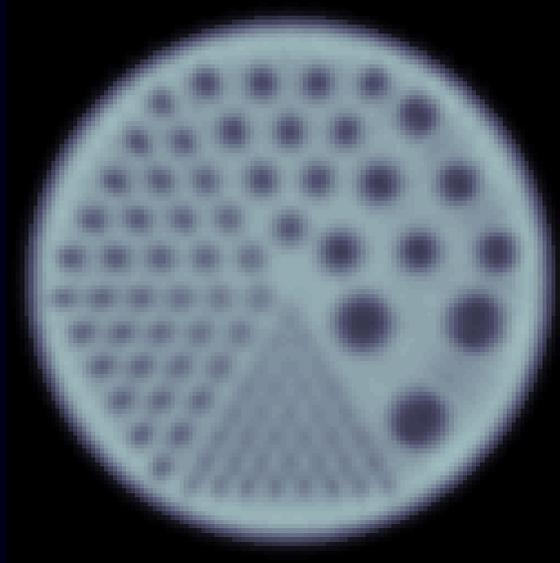
- a) filtered backprojection
- b) Penalized unweighted least-squares
- c) PWLS with conventional regularization
- d) PWLS with certainty-based penalty [25]
- e) PWLS with modified penalty [143]

Modified Penalty Example, SPECT - Noiseless

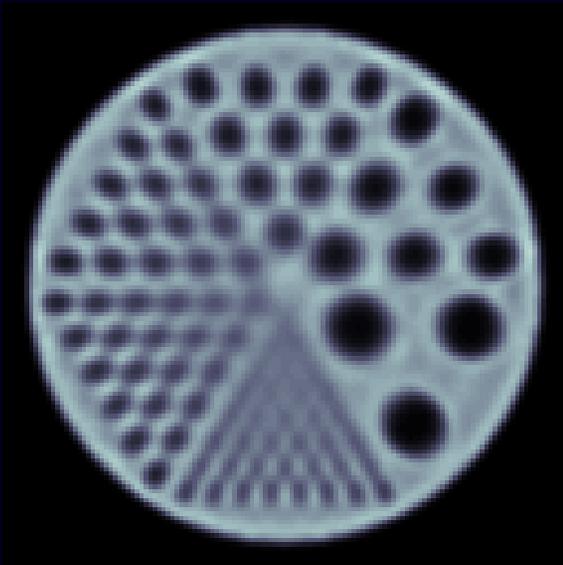
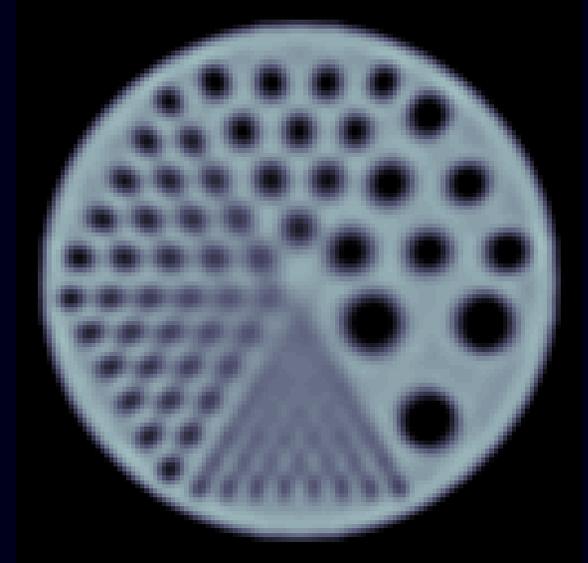
Target filtered object



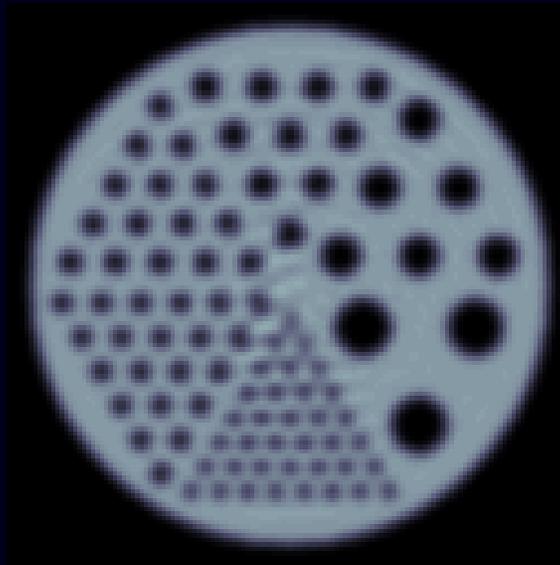
FBP



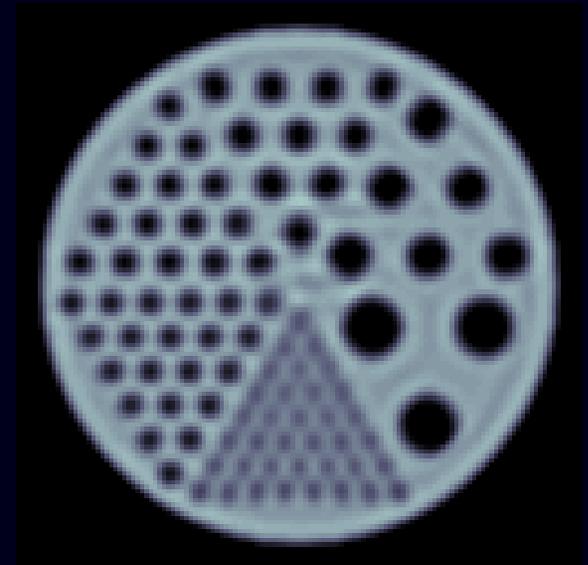
Conventional PWLS



Truncated EM



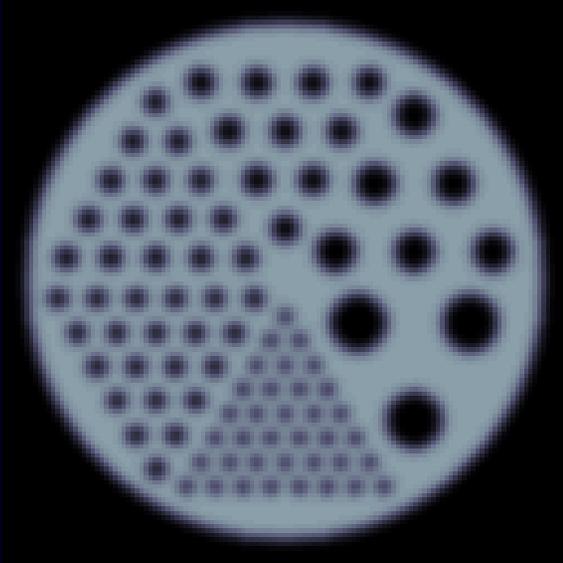
Post-filtered EM



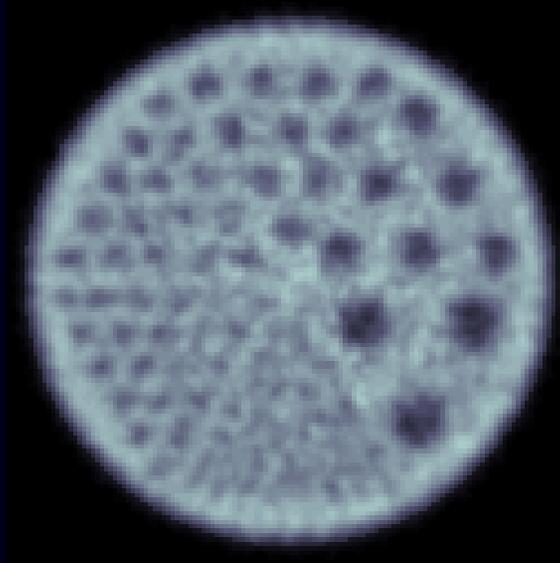
Modified Regularization

Modified Penalty Example, SPECT - Noisy

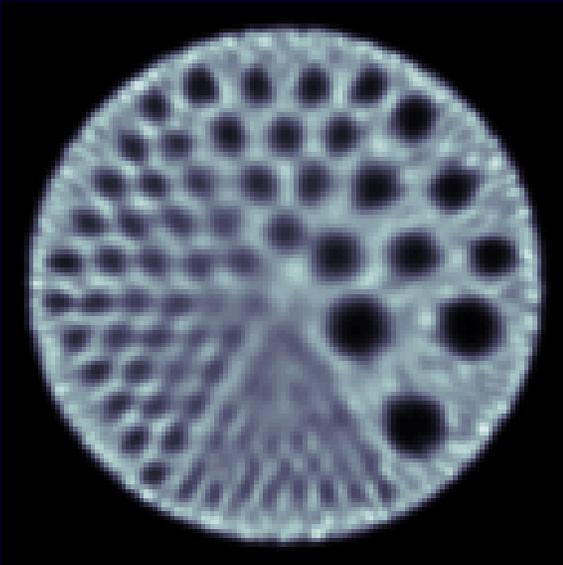
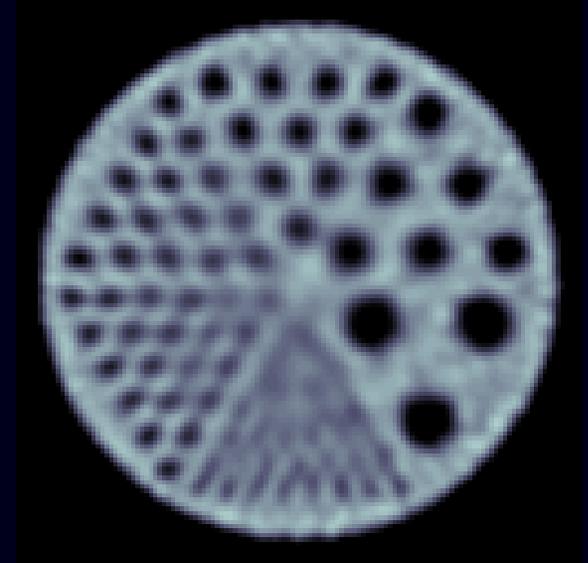
Target filtered object



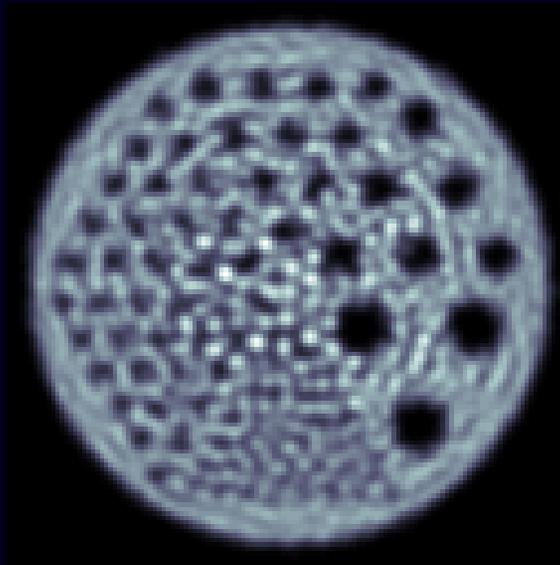
FBP



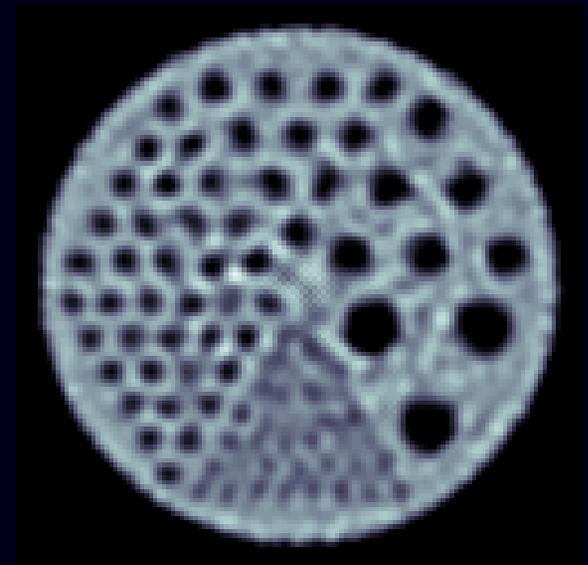
Conventional PWLS



Truncated EM



Post-filtered EM



Modified Regularization

Reconstruction Noise Properties

For unconstrained (converged) minimization methods, the estimator is *implicit*:

$$\hat{\mathbf{x}} = \hat{\mathbf{x}}(\mathbf{y}) = \arg \min_x \Psi(\mathbf{x}, \mathbf{y}).$$

What is $\text{Cov}\{\hat{\mathbf{x}}\}$?

New simpler derivation.

Denote the column gradient by $g(\mathbf{x}, \mathbf{y}) \triangleq \nabla_x \Psi(\mathbf{x}, \mathbf{y})$.

Ignoring constraints, the gradient is zero at the minimizer: $g(\hat{\mathbf{x}}(\mathbf{y}), \mathbf{y}) = \mathbf{0}$.

First-order Taylor series expansion:

$$\begin{aligned} g(\hat{\mathbf{x}}, \mathbf{y}) &\approx g(\mathbf{x}^{\text{true}}, \mathbf{y}) + \nabla_x g(\mathbf{x}^{\text{true}}, \mathbf{y})(\hat{\mathbf{x}} - \mathbf{x}^{\text{true}}) \\ &= g(\mathbf{x}^{\text{true}}, \mathbf{y}) + \nabla_x^2 \Psi(\mathbf{x}^{\text{true}}, \mathbf{y})(\hat{\mathbf{x}} - \mathbf{x}^{\text{true}}). \end{aligned}$$

Equating to zero:

$$\hat{\mathbf{x}} \approx \mathbf{x}^{\text{true}} - [\nabla_x^2 \Psi(\mathbf{x}^{\text{true}}, \mathbf{y})]^{-1} \nabla_x \Psi(\mathbf{x}^{\text{true}}, \mathbf{y}).$$

If the Hessian $\nabla^2 \Psi$ is weakly dependent on \mathbf{y} , then

$$\boxed{\text{Cov}\{\hat{\mathbf{x}}\} \approx [\nabla_x^2 \Psi(\mathbf{x}^{\text{true}}, \bar{\mathbf{y}})]^{-1} \text{Cov}\{\nabla_x \Psi(\mathbf{x}^{\text{true}}, \mathbf{y})\} [\nabla_x^2 \Psi(\mathbf{x}^{\text{true}}, \bar{\mathbf{y}})]^{-1} .}$$

If we further linearize w.r.t. the data: $g(\mathbf{x}, \mathbf{y}) \approx g(\mathbf{x}, \bar{\mathbf{y}}) + \nabla_y g(\mathbf{x}, \bar{\mathbf{y}})(\mathbf{y} - \bar{\mathbf{y}})$, then

$$\text{Cov}\{\hat{\mathbf{x}}\} \approx [\nabla_x^2 \Psi]^{-1} (\nabla_x \nabla_y \Psi) \text{Cov}\{\mathbf{y}\} (\nabla_x \nabla_y \Psi)' [\nabla_x^2 \Psi]^{-1} .$$

Covariance Continued

Covariance approximation:

$$\text{Cov}\{\hat{\mathbf{x}}\} \approx [\nabla_x^2 \Psi(\mathbf{x}^{\text{true}}, \bar{\mathbf{y}})]^{-1} \text{Cov}\{\nabla_x \Psi(\mathbf{x}^{\text{true}}, \mathbf{y})\} [\nabla_x^2 \Psi(\mathbf{x}^{\text{true}}, \bar{\mathbf{y}})]^{-1}$$

Depends only on chosen **cost function** and **statistical model**.
Independent of optimization algorithm.

- Enables prediction of noise properties
- Can make variance images
- Useful for computing ROI variance (*e.g.*, for weighted kinetic fitting)
- Good variance prediction for quadratic regularization in nonzero regions
- Inaccurate for nonquadratic penalties, or in nearly-zero regions

Qi and Huesman's Detection Analysis

SNR of MAP reconstruction $>$ SNR of FBP reconstruction (T-MI, Aug. 2001)

quadratic regularization

SKE/BKE task

prewhitened observer

non-prewhitened observer

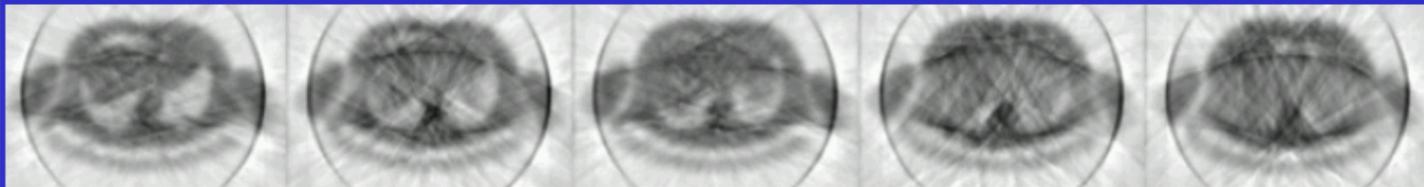
Part 5. Miscellaneous Topics

(Pet peeves and more-or-less recent favorites)

- Short transmission scans
- 3D PET options
- OSEM of transmission data (ugh!)
- Precorrected PET data
- Transmission scan problems
- List-mode EM
- List of other topics I wish I had time to cover...

PET Attenuation Correction (J. Nuyts)

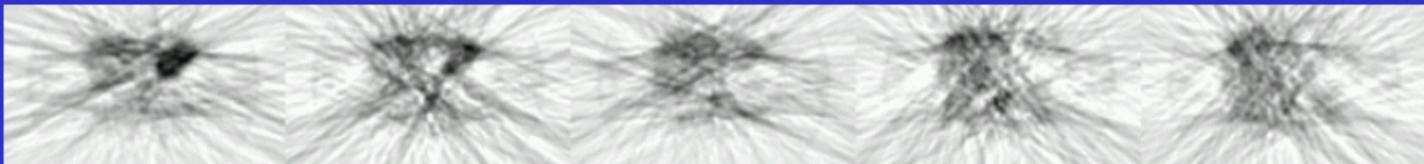
Short transmission scan



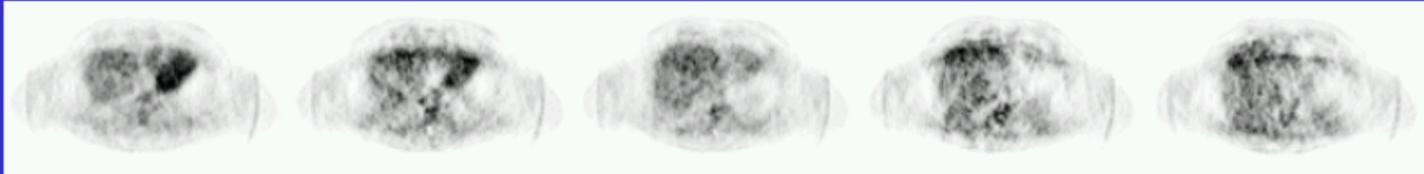
**Classic
Transm.**



**M.A.P
Reconstr.**



**•Classic
Atten cor
•FBP**



**•Classic
Atten cor
•MLEM**



**•M.A.P.
Atten cor
•MLEM**

Iterative reconstruction for 3D PET

- Fully 3D iterative reconstruction
- Rebinning / 2.5D iterative reconstruction
- Rebinning / 2D iterative reconstruction
 - PWLS
 - OSEM with attenuation weighting
- 3D FBP
- Rebinning / FBP

OSEM of Transmission Data?

Bai and Kinahan *et al.* “Post-injection single photon transmission tomography with ordered-subset algorithms for wholebody PET imaging”

- 3D penalty better than 2D penalty
- OSTR with 3D penalty better than FBP and OSEM
- standard deviation from a single realization to estimate noise can be misleading

Using OSEM for transmission data requires taking logarithm, whereas OSTR does not.

Precorrected PET data

C. Michel examined shifted-Poisson model, “weighted OSEM” of various flavors.
concluded attenuation weighting matters especially

Transmission Scan Challenges

- Overlapping-beam transmission scans
- Polyenergetic X-ray CT scans
- Sourceless attenuation correction

All can be tackled with optimization transfer methods.

List-mode EM

$$\begin{aligned}x_j^{(n+1)} &= x_j^{(n)} \left[\sum_{i=1}^{n_d} a_{ij} \frac{y_i}{\bar{y}_i^{(n)}} \right] / \left(\sum_{i=1}^{n_d} a_{ij} \right) \\ &= \frac{x_j^{(n)}}{\sum_{i=1}^{n_d} a_{ij}} \sum_{i: y_i \neq 0} a_{ij} \frac{y_i}{\bar{y}_i^{(n)}}\end{aligned}$$

- Useful when $\sum_{i=1}^{n_d} y_i \leq \sum_{i=1}^{n_d} 1$
- Attenuation and scatter non-trivial
- Computing a_{ij} on-the-fly
- Computing sensitivity $\sum_{i=1}^{n_d} a_{ij}$ still painful
- List-mode ordered-subsets is naturally balanced

Misc

- 4D regularization (reconstruction of dynamic image sequences)
- “Sourceless” attenuation-map estimation
- Post-injection transmission/emission reconstruction
- μ -value priors for transmission reconstruction
- Local errors in $\hat{\mu}$ propagate into emission image (PET and SPECT)

Summary

- Predictability of resolution / noise and controlling spatial resolution argues for regularized *cost function*
- todo: Still work to be done...

