

Jeffrey A. Fessler

EECS Department, BME Department, Dept. of Radiology University of Michigan http://web.eecs.umich.edu/~fessler **DOE Advanced Scientific Computing Research** Inverse Methods for Complex Systems under Uncertainty Workshop 2025-06-11 Acknowledgments: Jason Hu, Bowen Song, Xiaojian Xu, Liyue Shen arXiv 2406.02462 (NeurIPS 2024) arXiv 2406.10211 (NeurIPS 2024) arXiv 2410.11730 (in review)

Outline



Introduction

Inverse problems Generative models

Patch-based models

Non-overlapping patch model Patch Diffusion Inverse Solver (PaDIS) CT reconstruction results 3D CT reconstruction

Distribution shifts

Summary

Book

Bibliography

Under-determined inverse problems



Applications: compressed sensing MRI, sparse-view CT, PET, inpainting, ... All have *linear* forward models for data:

$$y = Ax + \varepsilon$$

- **y**: sensor data (*e.g.*, sinogram)
- A: wide system matrix (known)
- x: latent image (or image series in dynamic problems)
- ε : noise with known distribution provides likelihood p(y|x)
- Maximum-likelihood estimation (physics-based fitting) is usually non-unique:

$$\hat{\boldsymbol{x}} = \arg \max_{\boldsymbol{x}} \log p(\boldsymbol{y}|\boldsymbol{x}) = \arg \min_{\boldsymbol{x}} \|\boldsymbol{A}\boldsymbol{x} - \boldsymbol{y}\|_{2}^{2}$$
(for gaussian noise)

Minimum-norm least-squares solution is unique but usually impractical or useless:

$$\hat{\pmb{x}}=\pmb{A}^+\pmb{y}=\pmb{y}$$
 for inpainting problem

Inverse problem solution methods



hand-crafted regularizers:

$$\hat{\boldsymbol{x}} = \operatorname*{arg\,min}_{\boldsymbol{x}} - \log p(\boldsymbol{y}|\boldsymbol{x}) + R(\boldsymbol{x}) = \operatorname*{arg\,min}_{\boldsymbol{x}} \frac{1}{2\sigma_{\varepsilon}^2} \|\boldsymbol{A}\boldsymbol{x} - \boldsymbol{y}\|_2^2 + R(\boldsymbol{x})$$

.....

black-box data-driven supervised methods:

$$oldsymbol{A}^+oldsymbol{y} o oldsymbol{\mathsf{NN}} o oldsymbol{\hat{x}}$$

- unrolled deep learning methods (PNP, RED, MoDL, ...)
- Bayesian methods (e.g., MAP) based on a prior p(x), lately (?) relabeled as generative models (or "genAI")

Inverse problem solution methods



hand-crafted regularizers:

$$\hat{\boldsymbol{x}} = \operatorname*{arg\,min}_{\boldsymbol{x}} - \log p(\boldsymbol{y}|\boldsymbol{x}) + R(\boldsymbol{x}) = \operatorname*{arg\,min}_{\boldsymbol{x}} \frac{1}{2\sigma_{\varepsilon}^2} \|\boldsymbol{A}\boldsymbol{x} - \boldsymbol{y}\|_2^2 + R(\boldsymbol{x})$$

.....

black-box data-driven supervised methods:

$$oldsymbol{A}^+oldsymbol{y} o oldsymbol{\mathsf{NN}} o oldsymbol{\hat{x}}$$

- unrolled deep learning methods (PNP, RED, MoDL, ...)
- Bayesian methods (e.g., MAP) based on a prior p(x), lately (?) relabeled as generative models (or "genAI")
- Appeal:
 - \circ PNP-like training independent of \boldsymbol{A} or $p(\boldsymbol{y}|\boldsymbol{x})$
 - \circ Strong priors for complex systems with aggressive under-sampling
 - \circ Posterior sampling from $\mathsf{p}(\pmb{x}|\pmb{y})$ for uncertainty quantification

Long history of Bayesian models for inverse problems



Markov random field models

(*e.g.*) Geman & Geman 1984 [1]



(a)

GEMAN AND GEMAN: STOCHASTIC RELAXATION, GIBBS DISTRIBUTIONS, AND BAYESIAN RESTORATION

с. с.



(d)



Mostly for inference?

MRF as generators?

[2] T-PAMI 1994

An Empirical Study of the Simulation of Various Models Used for Images

A. J. Gray, J. W. Kay, and D. M. Titterington

Abstract— Markov random fields are typically used as priors in Bayesian image restoration methods to represent spatial information in the image. Commonly used Markov random fields are not in fact capable of representing the moderate-to-large scale clustering present in naturally occurring images and can also be time consuming to simulate,



(c)



J. Fessler

Patch models





(g)

Local vs global priors



Gray, Kay, Titterington [2] T-PAMI 1994 ... the local properties of spatial Markov models are undoubtedly plausible descriptors of the local associations typical of many images, which is the way in which the models are often used. Nevertheless. it would be reassuring if models used as priors did in fact provide a realistic representation of our prior assumptions and if their (empirical) properties were more widely known.



Fig. 4. Realizations of two-dimensional, one-parameter, autologistic Markov Mesh models: (a) binary, second-order model with $\beta = \log 5$; (b) three-color second-order model with $\beta = \log 5$; (c) binary second-order model with $\beta = \log 10$; (d) binary second-order model with $\beta = \log 3$.

Generative models are hot in imaging / inverse problems

J. Fessler Patch models

Zhao, Ye, Bresler: Jan. 2023 IEEE SpMag survey paper [3]

- Generative adversarial network (GAN) models
- Variation auto-encoder (VAE) models [4]
- Normalizing flows [5, 6]
- Score-based diffusion models
 - Zaccharie Ramzi et al., NeurIPS Workshop 2020 [7]
 - Yang Song & Liyue Shen et al., NeurIPS Workshop 2021, ICLR 2022 [8, 9]
 - \circ Ajil Jalal et al. ... Jon Tamir, NeurIPS 2021 [10]
 - \circ Hyungjin Chung & Jong Chul Ye, MIA, Aug. 2022 [11]
 - \circ Luo et al., MRM, 2023 [12]

o ...

- ► Kazerouni et al. [13] have github catalog, including >20 (!) survey papers
- ... (hopelessly incomplete lists)

Medical example: Low-dose sparse-view X-ray CT imaging

From Song & Shen et al., ICLR 2022 [9]. Trained with 47K 2D CT images. Recon 23 projection views (\approx 17-fold dose reduction)

 $\boldsymbol{A} = \mathcal{D}(\boldsymbol{\Lambda})\boldsymbol{T}$

$$\overbrace{\mathbf{X}}^{T} \xrightarrow{T} \underset{\text{Sinogram}}{\text{Sinogram}} \xrightarrow{\mathcal{P}(\mathbf{A})} \underset{\text{diag}(\mathbf{A})}{\mathcal{Y}}$$

PSNR: 20.30, SSIM: 0.778 PSNR: 22.94, SSIM: 0.552 PSNR: 22.78, SSIM: 0.603 PSNR: 31.76, SSIM: 0.882 PSNR: 35.23, SSIM: 0.912



(a) FISTA-TV (b) cGAN (c) Neumann (d) SIN-4c-PRN (e) Ours (f) Ground truth

J. Fessler

Patch models



- Learning whole-image prior models requires many high-quality training images Some applications like dynamic MRI have few *if any* realistic training samples
 Curse of dimensionality
 - Images live near manifolds (unsuitable for traditional density estimators)
 - \circ Implicit bias of model is crucial

2.



- Learning whole-image prior models requires many high-quality training images Some applications like dynamic MRI have few *if any* realistic training samples
 Curse of dimensionality
 - Images live near manifolds (unsuitable for traditional density estimators)
 - \circ Implicit bias of model is crucial
- 2. Existing models scale poorly to 3D or 3D+time
 - \circ GPU memory
 - \circ training data requirements

3.



- Learning whole-image prior models requires many high-quality training images Some applications like dynamic MRI have few *if any* realistic training samples
 Curse of dimensionality
 - Images live near manifolds (unsuitable for traditional density estimators)
 - $\circ\,$ Implicit bias of model is crucial
- 2. Existing models scale poorly to 3D or 3D+time
 - GPU memory
 - \circ training data requirements
- Training images should arise from relevant distribution p(x) Imaging-system aspects like X-ray source spectrum may cause domain shift

4.



- Learning whole-image prior models requires many high-quality training images Some applications like dynamic MRI have few *if any* realistic training samples
 Curse of dimensionality
 - Images live near manifolds (unsuitable for traditional density estimators)
 - $\circ\,$ Implicit bias of model is crucial
- 2. Existing models scale poorly to 3D or 3D+time
 - \circ GPU memory
 - \circ training data requirements
- Training images should arise from relevant distribution p(x) Imaging-system aspects like X-ray source spectrum may cause domain shift
- 4. What does "uncertainty" mean if prior is misspecified?

Challenge 1: Data availability

Whole images vs patches?



Jan. 2023 survey paper on generative models [3] does not mention "patch" once!?

MRI k-space sampling:



Patch-based models have long history in inverse problems, e.g.,

- patch GAN [17-19]
- patch dictionary models [20, 21]
- non-local means, BM3D
- Wasserstein patch prior [22, 23] ...



 Can patch-based generative models be effective priors for inverse problems in applications with very limited training data?
 e.g., dynamic MRI

Can patch-based generative models provide better robustness to distribution shifts, perhaps at the cost of reduced in-distribution performance?

Can we use the "latest" generative models, *e.g.*, score-based models, for patches?

Patch diffusion model: Simple version



Warm up:

simple, but less effective, approach:

- Fixed patch size
- Fixed patch grid

• No position information (Fessler, Hu, Xu, BASP 2023 [26])



Patch-based score modeling



Start with MRF formulation, aka *fields of experts* model [31–33] for image **x**:

$$\mathsf{p}(\boldsymbol{x};\boldsymbol{\theta}) = \frac{1}{Z(\boldsymbol{\theta})} e^{-\sum_{c} V_{c}(\boldsymbol{x};\boldsymbol{\theta})} = \frac{1}{Z(\boldsymbol{\theta})} \prod_{c} e^{-V_{c}(\boldsymbol{x};\boldsymbol{\theta})}.$$

- $oldsymbol{ heta}$: parameter vector that describes the prior
- V_c : clique potential for the cth image patch
- $Z(\theta)$: (intractable) partition function
- Assume (temporarily) statistical spatial stationarity (image shift invariance):

$$V_c(\boldsymbol{x}; \boldsymbol{\theta}) = V(\boldsymbol{G}_c \boldsymbol{x}; \boldsymbol{\theta})$$

- \boldsymbol{G}_c : wide binary matrix that grabs pixels of the cth patch from image \boldsymbol{x}
- $V(\mathbf{v}; \mathbf{\theta})$: common patch clique function

Patch-based score modeling (simple)



Resulting log-prior:

$$\log p(\boldsymbol{x}; \boldsymbol{\theta}) = -\log Z(\boldsymbol{\theta}) - \sum_{c} V(\boldsymbol{G}_{c}\boldsymbol{x}; \boldsymbol{\theta})$$

Corresponding overall *image score function* arises from *patch score function*:

$$\boldsymbol{s}(\boldsymbol{x};\boldsymbol{\theta}) \triangleq \nabla_{\boldsymbol{x}} \log p(\boldsymbol{x};\boldsymbol{\theta}) = \sum_{c} \boldsymbol{G}_{c}' \boldsymbol{s}_{V}(\boldsymbol{G}_{c}\boldsymbol{x};\boldsymbol{\theta}), \qquad \boldsymbol{s}_{V}(\boldsymbol{v};\boldsymbol{\theta}) \triangleq -\nabla_{\boldsymbol{v}} V(\boldsymbol{v};\boldsymbol{\theta}).$$

All we must learn is the patch score function s_V(v; θ) : ℝⁿ → ℝⁿ, e.g., a UNet.
 For non-overlapping patches:

$$\underbrace{\left\| \mathbf{s}(\mathbf{x} + \mathbf{z}; \boldsymbol{\theta}) + \mathbf{z}/\sigma^2 \right\|_2^2}_{\text{image "denoise"}} = \left\| \sum_c \mathbf{G}'_c \mathbf{s}_V (\mathbf{G}_c(\mathbf{x} + \mathbf{z}); \boldsymbol{\theta}) + \mathbf{z}/\sigma^2 \right\|_2^2}_{\text{patch "denoise"}} = \sum_c \underbrace{\left\| \mathbf{s}_V (\mathbf{x}_c + \mathbf{z}_c); \boldsymbol{\theta} \right\| + \mathbf{z}/\sigma^2 \right\|_2^2}_{\text{patch "denoise"}}, \quad \mathbf{z}_c \triangleq \mathbf{G}_c \mathbf{z}$$

Patch-based score learning (simple)



For training image patches {ν₁,..., ν_T}, apply *denoising score matching* (DSM) of Vincent, 2011 [34], typically for a range of noise variances σ² [35]:

$$\hat{\boldsymbol{\theta}} = \arg\min_{\boldsymbol{\theta}} \frac{1}{T} \sum_{t=1}^{T} \mathsf{E}_{\sigma \sim \boldsymbol{p}(\sigma)} \left[\sigma^2 \, \mathsf{E}_{\boldsymbol{z} \sim \mathcal{N}(\boldsymbol{0}, \sigma^2 \boldsymbol{I}_n)} \left[\frac{1}{2} \left\| \boldsymbol{s}_V(\boldsymbol{v}_t + \boldsymbol{z}; \boldsymbol{\theta}, \sigma) + \frac{\boldsymbol{z}}{\sigma^2} \right\|_2^2 \right] \right].$$

Final patch score model is $\mathbf{s}_V(\mathbf{v}; \hat{\mathbf{\theta}}, \sigma_{\min})$.

Patch-based score learning (simple)



For training image patches {ν₁,..., ν_T}, apply *denoising score matching* (DSM) of Vincent, 2011 [34], typically for a range of noise variances σ² [35]:

$$\hat{\boldsymbol{\theta}} = \arg\min_{\boldsymbol{\theta}} \frac{1}{T} \sum_{t=1}^{T} \mathsf{E}_{\sigma \sim \boldsymbol{\rho}(\sigma)} \left[\sigma^2 \, \mathsf{E}_{\boldsymbol{z} \sim \mathcal{N}(0, \sigma^2 \boldsymbol{I}_n)} \left[\frac{1}{2} \left\| \boldsymbol{s}_V(\boldsymbol{v}_t + \boldsymbol{z}; \boldsymbol{\theta}, \sigma) + \frac{\boldsymbol{z}}{\sigma^2} \right\|_2^2 \right] \right].$$

Final patch score model is $\boldsymbol{s}_{V}(\boldsymbol{v}; \hat{\boldsymbol{\theta}}, \sigma_{\min})$.

Network input is just image patches, never the entire image scales to large 2D images, 3D, 4D, etc.

Patch-based score learning (simple)



For training image patches {ν₁,..., ν_T}, apply *denoising score matching* (DSM) of Vincent, 2011 [34], typically for a range of noise variances σ² [35]:

$$\hat{\boldsymbol{\theta}} = \arg\min_{\boldsymbol{\theta}} \frac{1}{T} \sum_{t=1}^{T} \mathsf{E}_{\sigma \sim \boldsymbol{\rho}(\sigma)} \left[\sigma^{2} \, \mathsf{E}_{\boldsymbol{z} \sim \mathcal{N}(0, \sigma^{2} \boldsymbol{I}_{n})} \left[\frac{1}{2} \left\| \boldsymbol{s}_{V}(\boldsymbol{v}_{t} + \boldsymbol{z}; \boldsymbol{\theta}, \sigma) + \frac{\boldsymbol{z}}{\sigma^{2}} \right\|_{2}^{2} \right] \right].$$

Final patch score model is $\mathbf{s}_V(\mathbf{v}; \hat{\boldsymbol{\theta}}, \sigma_{\min})$.

- Network input is just image patches, never the entire image scales to large 2D images, 3D, 4D, etc.
- Drawbacks:
 - \circ Visible patch boundaries
 - \circ Fixed patch size slows learning
 - Suboptimal stationarity assumption (cf. vertebrae)

Improved patch modeling





Probability model with padding & grids & positions



- $N_1 \times N_2$: original image size
- ▶ $P_1 \times P_2$: patch size
- ▶ $K_i \triangleq 1 + \lfloor N_i / P_i \rfloor$, i = 1, 2: # non-overlapping patches for original image
- $(N_1 + 2M_1) \times (N_2 + 2M_2)$: padded image size; $M_i \triangleq K_i P_i N_i$
- Product probability model:



 $\circ \mathbf{x}_{m,B} : \text{ border pixels for } m\text{th shift (all zero)} \\ \circ \mathbf{x}_{m,k} : k\text{th patch for } m\text{th shift}$

Probability model with padding & grids & positions



- $N_1 \times N_2$: original image size
- ▶ $P_1 \times P_2$: patch size
- ▶ $K_i \triangleq 1 + \lfloor N_i / P_i \rfloor$, i = 1, 2: # non-overlapping patches for original image
- $(N_1 + 2M_1) \times (N_2 + 2M_2)$: padded image size; $M_i \triangleq K_i P_i N_i$
- Product probability model:



- $\circ \mathbf{x}_{m,B}$: border pixels for *m*th shift (all zero)
- $\circ \mathbf{x}_{m,k}$: kth patch for mth shift

Learn position-dependent patch score function $s(\mathbf{v}; \mathbf{\theta}, m, k) = -\nabla_{\mathbf{v}} V(\mathbf{v}; m, k)$

Patch Diffusion Inverse Solver (PaDIS): Training





NeurIPS 2024 [42] arXiv 2406.02462

Training images (CT)



AAPM 2016 CT challenge data [43]; 10 3D volumes, rescaled to 256³

Example slices:



Image generation (unconditional sampling from prior)





- \circ Top: generation with a network trained on whole images (2D...)
- \circ Middle: patch-only version of [40] (non-overlapping patches).
- \circ Bottom: generation with proposed PaDIS prior.



2 A40 GPUs using PyTorch and ADAM

- ▶ whole image model: 24 36 hours
- \blacktriangleright patch-based model: ≈ 12 hours

Patch Diffusion Inverse Solver (PaDIS): Reconstruction





Diffusion posterior sampling (DPS) (Chung et al., ICLR 2023 [44]) with Langevin dynamics, modified to use patch score with random grid shifts.

PaDIS algorithm (modified from DPS)



Input: $\boldsymbol{y}, \boldsymbol{A}, T, \sigma_1 < \sigma_2 < \ldots < \sigma_T, \epsilon > 0, \{\zeta_t > 0\}, P_1, P_2, M_1, M_2,$ trained noise-conditional, position-encoded patch denoiser $\boldsymbol{d}(\cdot; \boldsymbol{\theta}_*, m, k, \sigma)$ Initialize random image $\boldsymbol{x} \sim \mathcal{N}(\boldsymbol{0}, \sigma_T^2 \boldsymbol{I})$

for t = T : 1 do

Randomly select grid integer $m \in \{1, \ldots, M_1 M_2\}$

for k = 1: (K_1K_2) do (parallelizable)

Extract patch $\boldsymbol{x}_{m,k}$

Denoise patch: $\boldsymbol{d}_{m,k} \triangleq \boldsymbol{d}(\boldsymbol{x}_{m,k}; \boldsymbol{\theta}_*, m, k, \sigma_t)$

end for

Combine denoised patches to get denoised image dCompute image score function: $\mathbf{s} = (\mathbf{d} - \mathbf{x})/\sigma_t^2$ Data term: $\mathbf{x} := \mathbf{x} - \zeta_t \nabla_{\mathbf{x}} \| \mathbf{A} \, \mathbf{d}(\mathbf{x}) - \mathbf{y} \|_2^2$ Sample $\mathbf{z} \sim \mathcal{N}(\mathbf{0}, \sigma_t^2 \mathbf{I})$ Step size $\alpha_t \triangleq \epsilon \sigma_t^2$ Langevin update: $\mathbf{x} := \mathbf{x} + \frac{\alpha_t}{2}\mathbf{s} + \sqrt{\alpha_t}\mathbf{z}$ end for



Default setup:

- 9 of 10 volumes for training \Longrightarrow 2304 slices
- 25 slices of 10th volume for testing
- 512 element parallel-beam CT detector
- A from Operator Discretization Library (ODL)
- 56 imes 56 patch size
- U-Net of Karras 2022 [41]
- Step size $\zeta_t = \zeta/\|oldsymbol{Ad}(oldsymbol{x}_t) oldsymbol{y}\|_2$
- 1000 neural function evaluations (NFEs) [41]



Mathad	CT, 20 Views		CT, 8 Views		Deblurring		Superresolution	
Method	PSNR↑	SSIM↑	PSNR↑	SSIM↑	PSNR↑	SSIM↑	PSNR↑	SSIM↑
Baseline	24.93	0.595	21.39	0.415	24.54	0.688	25.86	0.739
ADMM-TV	26.82	0.724	23.09	0.555	28.22	0.792	25.66	0.745
PnP-ADMM [45]	26.86	0.607	22.39	0.489	28.82	0.818	26.61	0.785
PnP-RED [46]	27.99	0.622	23.08	0.441	29.91	0.867	26.36	0.766
Whole image diffusion	32.84	0.835	25.74	0.706	30.19	0.853	29.17	0.827
Langevin dynamics [47]	33.03	0.846	27.03	0.689	30.60	0.867	26.83	0.744
Predictor-corrector [11]	32.35	0.820	23.65	0.546	28.42	0.724	26.97	0.685
VE-DDNM [48]	31.98	0.861	27.71	0.759	-	-	26.01	0.727
Patch Averaging [30]	33.35	0.850	28.43	0.765	29.41	0.847	27.67	0.802
Patch Stitching	32.87	0.837	26.71	0.710	29.69	0.849	27.50	0.780
PaDIS (Ours)	33.57	0.854	29.48	0.767	30.80	0.870	29.47	0.846

(Averages across all test images.)



Mathad	CT, 60	Views	vs CT, Fan Beam		Heavy Deblurring		
Method	PSNR↑	SSIM↑	PSNR↑	SSIM↑	PSNR↑	SSIM↑	
Baseline	25.89	0.746	20.07	0.521	21.14	0.569	
ADMM-TV	30.93	0.833	25.78	0.719	26.03	0.724	
Whole image diffusion	35.83	0.894	26.89	0.835	28.35	0.808	
PaDIS (Ours)	39.28	0.941	29.91	0.932	28.91	0.818	

Example images





Top: 60 view CT Bottom: fan-beam CT

 \approx 400 HU window width $_{_{\rm 29/56}}$



Patchsize

Positional encoding

Р	PSNR↑	SSIM↑
8	32.57	0.844
16	32.57	0.829
32	32.72	0.853
56	33.57	0.854
96	33.36	0.854
256	32.84	0.835

	PSNR↑	SSIM↑
no position enc.	23.25	0.459
no position+init	24.51	0.518
with position	33.57	0.854



Dataset	Pato	ches	Whole image			
size	56 ×	< 56	256 imes256			
	PSNR↑ SSIM↑		PSNR↑	SSIM↑		
144	32.28	0.841	29.12	0.804		
288	32.43	0.837	31.09	0.829		
576	33.03	0.846	31.81	0.835		
1152	33.01	0.849	31.36	0.834		
2304	33.57	0.854	32.84	0.835		

20 view CT reconstruction: training dataset sizes





Top : PaDIS Bottom : whole image diffusion model Challenge 2: Data dimensions & scaling to 3D (and 4D)



arXiv 2406.10211 (NeurIPS 2024)



DiffusionBlend models groups of slices







Method	Distribution Model
DiffusionMBIR (2D) [49]	$\frac{1}{Z}\prod_{i=1}^{H}p(\boldsymbol{x}[:,:,i])$
TPDM (\perp 2D) [50]	$rac{1}{Z} \left(\prod_{i=1}^{N} q_{ heta}(oldsymbol{x}[:,:,i])^lpha ight) \left(\prod_{j=1}^{N} q_{\phi}(oldsymbol{x}[j,:,:])^eta ight)$
DiffusionBlend	$\frac{1}{Z} \prod_{i=1}^{H} p(\mathbf{x}[:,:,i] \mathbf{x}[:,:,i-j:i-1], \mathbf{x}[:,:,i+1:i+j])$
DiffusionBlend++	$\frac{1}{Z}\prod_{i=1}^{r}p(\mathbf{x}[:,:,\mathcal{S}_{i}])$





Improved quality both qualitatively and quantitively with strong prior.

Challenge 3: Distribution shifts



Test-time latent \boldsymbol{x} far from training distribution:

$$oldsymbol{y} = oldsymbol{A}oldsymbol{x} + arepsilon, \quad oldsymbol{x} \sim \widetilde{\mathsf{p}}(\cdot)
eq \mathsf{p}(\cdot)$$

Non-Bayes approach Abandon training via self-supervision, *e.g.*, deep image prior (DIP) [51]:

$$\hat{\pmb{x}} = f_{\hat{\pmb{ heta}}}(\pmb{z}), \qquad \hat{\pmb{ heta}} = \argmin_{\pmb{ heta}} \|\pmb{y} - \pmb{A} f_{\pmb{ heta}}(\pmb{z})\|_2^2, \qquad \pmb{z} \sim \mathcal{N}(\pmb{0}, \pmb{I})$$

Neural network $f_{\theta}(\cdot)$ acts as implicit regularizer. DIP is prone to overfitting of noisy measurements [51]; remedies such as early stopping, regularization, network initialization [52–54].



Self-supervised (whole-image) diffusion models [55, 56]
 "Deep diffusion image prior" (DDIP) or "steerable conditional diffusion:"

$$L(\boldsymbol{\theta}) = \|\boldsymbol{y} - \boldsymbol{A} \operatorname{CG}(\hat{\boldsymbol{x}}_{0|t}(\boldsymbol{x}_t; \boldsymbol{\theta}))\|_2^2$$

$$\operatorname{CG}(\hat{\boldsymbol{x}}_{0|t}) \triangleq \arg\min_{\boldsymbol{x}} \frac{\gamma}{2} \|\boldsymbol{y} - \boldsymbol{A}\boldsymbol{x}\|_2^2 + \frac{1}{2} \|\boldsymbol{x} - \hat{\boldsymbol{x}}_{0|t}\|_2^2$$

Conjugate gradient (CG) descent is used to enforce data fidelity. Still requires early stopping to avoid over-fitting.



Patch-based test-time adaptation [57, 58] arXiv 2410.11730 (in review) Test-time loss for diffusion model adaptation:

$$L(\theta) = \left\| \boldsymbol{y} - \boldsymbol{A} \sum_{c} \boldsymbol{G}'_{c} D_{\theta}(\boldsymbol{G}_{c} \boldsymbol{x}_{t}, c | \boldsymbol{y}) \right\|_{2}^{2}$$

Patch-based denoiser for diffusion model

$$D_{\boldsymbol{\theta}}(\boldsymbol{x}) = \sum_{c} \boldsymbol{G}'_{c} D_{\boldsymbol{\theta}}(\boldsymbol{G}_{c} \boldsymbol{x}, c),$$

Patch-based test-time adaptation II





No in-distribution training data. Pre-trained with random ellipses. Results of 60-view CT reconstruction using self supervised (SS) loss.



42 / 56



Method	CT, 20	Views	CT, 60 Views		Deblurring		Superresolution	
	PSNR↑	SSIM↑	PSNR↑	SSIM↑	PSNR↑	SSIM↑	PSNR↑	SSIM↑
Baseline	24.93	0.613	30.15	0.784	23.93	0.666	25.42	0.724
ADMM-TV	26.81	0.750	31.14	0.862	27.58	0.773	25.22	0.729
PnP-ADMM [45]	30.20	0.838	36.75	0.932	28.98	0.815	27.29	0.796
PnP-RED [46]	27.12	0.682	32.68	0.876	28.37	0.793	27.73	0.809
Whole image	28.11	0.800	33.10	0.911	25.85	0.742	25.65	0.742
Patches [42]	27.44	0.719	33.97	0.934	26.77	0.782	26.12	0.759
Whole+SS [56]	33.19	0.861	40.47	0.957	29.50	0.831	27.07	0.701
Patches+SS (Ours)	33.77	0.874	41.45	0.969	30.34	0.860	28.10	0.827

"SS" = self-supervision, aka test-time adaptation

Patch-based test-time adaptation IV





Towards a "universal" diffusion model



Extension to cases where # of channels at test time differs from training data, e.g., MR reconstruction (real/imag) from patch-based diffusion model pre-trained on color (RGB) natural images and grayscale CT images [59]



SPAR results





46 / 56



somparison of quantitative results on four unrefert medical imaging inverse problems.									
Mathad	PBCT,	60 Views	FBCT, 40 Views		512 imes 5	512×512 CT		CS-MRI, $7 \times$	
Method	PSNR↑	SSIM↑	PSNR↑	SSIM↑	PSNR↑	SSIM↑	PSNR↑	SSIM↑	
Baseline	30.15	0.784	17.86	0.381	28.33	0.700	33.94	0.894	
ADMM-TV	31.14	0.862	24.20	0.628	29.36	0.788	36.74	0.924	
PnP-ADMM [45]	36.75	0.932	28.86	0.747	37.48	0.910	35.77	0.907	
PaDIS+FC [42]	39.16	0.942	27.91	0.796	33.11	0.831	35.17	0.904	
SCD [56]	41.16	0.962	21.28	0.463	-	-	-	-	
Ours (SPAR)	42.72	0.972	36.11	0.918	38.81	0.929	39.15	0.949	
Ideal*	42.82	0.973	36.34	0.923	38.94	0.930	39.42	0.953	

Comparison of quantitative results on four different medical imaging inverse problems.

*not available in practice with a single diffusion model

Summary / future directions



- Challenges
 - Dearth of data
 - Dimensionality
 - Distribution shifts
- Promise
 - Generative models are promising for under-determined inverse problems
 - Learning patch score models is feasible with denoising score matching
 - For limited training data, patch-models can outperform whole-image models
- Future steps
 - Integrate invariances: amplitude scale / rotation / flip / DC offset ...
 - Explore trade-offs between generalizability and in-distribution performance
 - Extend to 3D, 3D+Time, 3D+Multicontrast

Tutorial Julia code: https://github.com/JeffFessler/ScoreMatching.jl

New book



Linear Algebra for Data Science, Machine Learning, and Signal Processing JEFFREY A. FESSLER RAJ RAO NADAKUDITI

- Online demos: https://github.com/JeffFessler/ book-la-demo
- Topics include: low-rank matrix approximation, robust PCA, photometric stereo, video foreground/background separation, spectral clustering, matrix completion, ...
- Available from Cambridge Univ. Press

Resources



Talk and code available online at http://web.eecs.umich.edu/~fessler



Bibliography I



- S. Geman and D. Geman. "Stochastic relaxation, Gibbs distributions, and Bayesian restoration of images." In: IEEE Trans. Patt. Anal. Mach. Int. 6.6 (Nov. 1984), 721–41.
- [2] A. J. Gray, J. W. Kay, and D. M. Titterington. "An empirical study of the simulation of various models used for images." In: IEEE Trans. Patt. Anal. Mach. Int. 16.5 (May 1994), 507–12.
- [3] Z. Zhao, J. C. Ye, and Y. Bresler. "Generative models for inverse imaging problems: from mathematical foundations to physics-driven applications." In: IEEE Sig. Proc. Mag. 40.1 (Jan. 2023), 148–63.
- [4] E. D. Zhong, T. Bepler, B. Berger, and J. H. Davis. "CryoDRGN: reconstruction of heterogeneous cryo-EM structures using neural networks." In: Nature Meth. 18.2 (2021), 176–85.
- [5] D. Rezende and S. Mohamed. "Variational inference with normalizing flows." In: Proc. Intl. Conf. Mach. Learn. 2015, 1530-8.
- [6] F. Altekruger, A. Denker, P. Hagemann, J. Hertrich, P. Maass, and G. Steidl. "PatchNR: learning from very few images by patch normalizing flow regularization." In: *Inverse Prob.* 39.6 (May 2023), p. 064006.
- [7] Z. Ramzi, B. Remy, F. Lanusse, J-L. Starck, and P. Ciuciu. "Denoising score-matching for uncertainty quantification in inverse problems." In: NeurIPS 2020 Workshop on Deep Learning and Inverse Problems. 2020.
- Y. Song, L. Shen, L. Xing, and S. Ermon. "Solving inverse problems in medical imaging with score-based generative models." In: NeurIPS Deep Inv. Work. 2021.
- Y. Song, L. Shen, L. Xing, and S. Ermon. "Solving inverse problems in medical imaging with score-based generative models." In: Proc. Intl. Conf. on Learning Representations. 2022.
- [10] A. Jalal, M. Arvinte, G. Daras, E. Price, A. Dimakis, and J. Tamir. "Robust compressed sensing MR imaging with deep generative priors." In: NeurIPS Workshop Deep Inverse. 2021.
- [11] H. Chung and J. C. Ye. "Score-based diffusion models for accelerated MRI." In: Med. Im. Anal. 80 (Aug. 2022), p. 102479.

Bibliography II



- [12] G. Luo, M. Blumenthal, M. Heide, and M. Uecker. "Bayesian MRI reconstruction with joint uncertainty estimation using diffusion models." In: Mag. Res. Med. 90.1 (July 2023), 295–311.
- [13] A. Kazerouni, E. K. Aghdam, M. Heidari, R. Azad, M. Fayyaz, I. Hacihaliloglu, and D. Merhof. "Diffusion models in medical imaging: A comprehensive survey." In: Med. Im. Anal. 88 (Aug. 2023), p. 102846.
- [14] G. Wang, T. Luo, J-F. Nielsen, D. C. Noll, and J. A. Fessler. "B-spline parameterized joint optimization of reconstruction and k-space trajectories (BJORK) for accelerated 2D MRI." In: IEEE Trans. Med. Imag. 41.9 (Sept. 2022), 2318–30.
- [15] W. Wu and K. L. Miller. "Image formation in diffusion MRI: A review of recent technical developments." In: J. Mag. Res. Im. 46.3 (Sept. 2017), 646–62.
- [16] S. Bhadra, W. Zhou, and M. A. Anastasio. "Medical image reconstruction with image-adaptive priors learned by use of generative adversarial networks." In: Proc. SPIE 11312 Medical Imaging: Phys. Med. Im. 2020, p. 113120V.
- [17] C. Li and M. Wand. "Precomputed real-time texture synthesis with Markovian generative adversarial networks." In: Proc. European Comp. Vision Conf. 2016, 702–16.
- [18] P. Isola, J-Y. Zhu, T. Zhou, and A. A. Efros. "Image-to-image translation with conditional adversarial networks." In: Proc. IEEE Conf. on Comp. Vision and Pattern Recognition. 2017, 5967–76.
- [19] A. Elnekave and Y. Weiss. "Generating natural images with direct patch distributions matching." In: Proc. European Comp. Vision Conf. Vol. 13677. 2022.
- [20] M. Aharon, M. Elad, and A. Bruckstein. "K-SVD: an algorithm for designing overcomplete dictionaries for sparse representation." In: IEEE Trans. Sig. Proc. 54.11 (Nov. 2006), 4311–22.
- [21] S. Ravishankar and Y. Bresler. "MR image reconstruction from highly undersampled k-space data by dictionary learning." In: IEEE Trans. Med. Imag. 30.5 (May 2011), 1028–41.

Bibliography III



- [22] J. Hertrich, A. Houdard, and C. Redenbach. "Wasserstein patch prior for image superresolution." In: IEEE Trans. Computational Imaging 8 (2022), 693–704.
- [23] F. Altekruger and J. Hertrich. "WPPNets and WPPFlows: The power of Wasserstein patch priors for superresolution." In: SIAM J. Imaging Sci. 16.3 (2023), 1033–67.
- [24] G. Vaksman, M. Zibulevsky, and M. Elad. "Patch ordering as a regularization for inverse problems in image processing." In: SIAM J. Imaging Sci. 9.1 (2016), 287–319.
- [25] M. Piening, F. Altekruger, J. Hertrich, P. Hagemann, A. Walther, and G. Steidl. Learning from small data sets: Patch-based regularizers in inverse problems for image reconstruction. 2023.
- [26] J. A. Fessler, J. Hu, and X. Xu. "Generalizability (or not?) of patch-based image models." In: BASP. Invited presentation. 2023.
- [27] U. S. Kamilov, E. Bostan, and M. Unser. "Variational justification of cycle spinning for wavelet-based solutions of inverse problems." In: IEEE Signal Proc. Letters 21.11 (Nov. 2014), 1326–30.
- [28] A. Saucedo, S. Lefkimmiatis, N. Rangwala, and K. Sung. "Improved computational efficiency of locally low rank MRI reconstruction using iterative random patch adjustments." In: IEEE Trans. Med. Imag. 36.6 (2017), 1209–20.
- [29] J. L. Rumberger, X. Yu, P. Hirsch, M. Dohmen, V. E. Guarino, A. Mokarian, L. Mais, J. Funke, and D. Kainmueller. "How shift equivariance impacts metric learning for instance segmentation." In: Proc. Intl. Conf. Comp. Vision. 2021, 7108–16.
- [30] O. Ozdenizci and R. Legenstein. "Restoring vision in adverse weather conditions with patch-based denoising diffusion models." In: IEEE Trans. Patt. Anal. Mach. Int. 45.8 (Jan. 2023), 10346–57.
- [31] G. E. Hinton. "Training products of experts by minimizing contrastive divergence." In: Neural Computation 14.8 (Aug. 2002), 1771-800.
- [32] S. Roth and M. J. Black. "Fields of experts." In: Intl. J. Comp. Vision 82.2 (Jan. 2009), 205-29.
- [33] D. P. Kingma and Y. LeCun. "Regularized estimation of image statistics by score matching." In: NeurIPS. 2010, 1126–34.

Bibliography IV



- [34] P. Vincent. "A connection between score matching and denoising autoencoders." In: Neural Comput. 23.7 (July 2011), 1661–74.
- [35] Y. Song, J. Sohl-Dickstein, D. P. Kingma, A. Kumar, S. Ermon, and B. Poole. "Score-based generative modeling through stochastic differential equations." In: Proc. Intl. Conf. on Learning Representations. 2021.
- [36] R. R. Coifman and D. L. Donoho. Translation-invariant denoising. 1995.
- [37] M. A. T. Figueiredo and R. D. Nowak. "An EM algorithm for wavelet-based image restoration." In: IEEE Trans. Im. Proc. 12.8 (Aug. 2003), 906–16.
- [38] U. Kamilov, E. Bostan, and M. Unser. "Wavelet shrinkage with consistent cycle spinning generalizes total variation denoising." In: IEEE Signal Proc. Letters 19.4 (Apr. 2012), 187–90.
- [39] F. Ong and M. Lustig. "Beyond low rank + sparse: multiscale low rank matrix decomposition." In: IEEE J. Sel. Top. Sig. Proc. 10.4 (June 2016), 672–87.
- [40] Z. Wang, Y. Jiang, H. Zheng, P. Wang, P. He, Z. Wang, W. Chen, and M. Zhou. "Patch diffusion: faster and more data-efficient training of diffusion models." In: *NeurIPS*. Vol. 36. 2023, 72137–54.
- [41] T. Karras, M. Aittala, T. Aila, and S. Laine. "Elucidating the design space of diffusion-based generative models." In: NeurIPS. 2022.
- [42] J. Hu, B. Song, X. Xu, L. Shen, and J. A. Fessler. "Learning image priors through patch-based diffusion models for solving inverse problems." In: NeurIPS. 2024.
- [43] C. H. McCollough, A. C. Bartley, R. E. Carter, B. Chen, T. A. Drees, P. Edwards, D. R. Holmes, A. E. Huang, F. Khan, S. Leng, K. L. McMillan, G. J. Michalak, K. M. Nunez, L. Yu, and J. G. Fletcher. "Low-dose CT for the detection and classification of metastatic liver lesions: Results of the 2016 Low Dose CT Grand Challenge." In: *Med. Phys.* 44.10 (Oct. 2017), e339–52.
- [44] H. Chung, J. Kim, M. T. Mccann, M. L. Klasky, and J. C. Ye. "Diffusion posterior sampling for general noisy inverse problems." In: Proc. Intl. Conf. on Learning Representations. 2023.

Bibliography V



- [45] X. Xu, J. Liu, Y. Sun, B. Wohlberg, and U. S. Kamilov. "Boosting the performance of plug-and-play priors via denoiser scaling." In: Proc., IEEE Asilomar Conf. on Signals, Systems, and Comp. 2020, 1305–12.
- [46] Y. Hu, J. Liu, X. Xu, and U. S. Kamilov. "Monotonically convergent regularization by denoising." In: Proc. IEEE Intl. Conf. on Image Processing. 2022, 426–30.
- [47] Y. Song and S. Ermon. "Generative modeling by estimating gradients of the data distribution." In: NeurIPS. 2019.
- [48] Y. Wang, J. Yu, and J. Zhang. "Zero-shot image restoration using denoising diffusion null-space model." In: Proc. Intl. Conf. Mach. Learn. 2023.
- [49] H. Chung, D. Ryu, M. T. McCann, M. L. Klasky, and J. C. Ye. "Solving 3D inverse problems using pre-trained 2D diffusion models." In: Proc. IEEE Conf. on Comp. Vision and Pattern Recognition. 2023, 22542–51.
- [50] S. Lee, H. Chung, M. Park, J. Park, W-S. Ryu, and J. C. Ye. "Improving 3D imaging with pre-trained perpendicular 2D diffusion models." In: Proc. Intl. Conf. Comp. Vision. 2023.
- [51] D. Ulyanov, A. Vedaldi, and V. Lempitsky. "Deep image prior." In: Proc. IEEE Conf. on Comp. Vision and Pattern Recognition. 2018, 9446–54.
- [52] J. Liu, Y. Sun, X. Xu, and U. S. Kamilov. "Image restoration using total variation regularized deep image prior." In: Proc. IEEE Conf. Acoust. Speech Sig. Proc. 2019, 7715–9.
- [53] Y. Jo, S. Y. Chun, and J. Choi. "Rethinking deep image prior for denoising." In: Proc. Intl. Conf. Comp. Vision. 2021, 5067-76.
- [54] R. Barbano, J. Leuschner, M. Schmidt, A. Denker, A. Hauptmann, P. Maass, and B. Jin. "An educated warm start for deep image prior-based micro CT reconstruction." In: IEEE Trans. Computational Imaging 8 (2022), 1210–22.
- [55] H. Chung and J. C. Ye. "Deep diffusion image prior for Efficient OOD adaptation in 3D inverse problems." In: Proc. European Comp. Vision Conf. 2024, 432–55.



- [56] R. Barbano, A. Denker, H. Chung, T. H. Roh, S. Arrdige, P. Maass, B. Jin, and J. C. Ye. "Steerable conditional diffusion for out-of-distribution adaptation in imaging inverse problems." In: *IEEE Trans. Med. Imag.* 44.5 (May 2025), 2093–104.
- [57] J. Hu, B. Song, J. A. Fessler, and L. Shen. Patch-based diffusion models beat whole-image models for mismatched distribution inverse problems. 2024.
- [58] J. Hu, B. Song, J. A. Fessler, and L. Shen. "Test-time adaptation improves inverse problem solving with patch-based diffusion models." In: IEEE Trans. Computational Imaging (2025). Submitted.
- [59] J. Hu, Z. Li, B. Song, L. Shen, and J. A. Fessler. "SPAR: refining a single pretrained diffusion model to solve inverse problems in many modalities." In: NeurIPS. 2025.