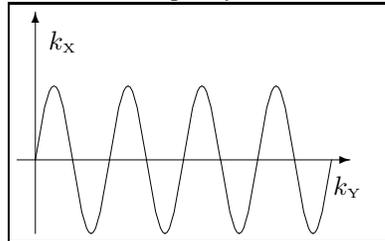


Homework #5, EECS 516, F09. Due **Due Fri. Oct. 30**, by 1:30PM**MR physics**

1. [10] Let the total number of spins per unit volume be $N = N_+ + N_-$, for $I_z = \pm 1/2$.
- (a) [5] Find an expression for $E[N_+ - N_-]$ in terms of N and the physical parameters.
- (b) [5] When kT is large relative to the energy difference between the two spin states, simplify your answer to part (a).
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2. [15] Consider two materials A and B having the same equilibrium magnetization M_{z0} , but with relaxation parameters (T_{1A}, T_{2A}) and (T_{1B}, T_{2B}) respectively. For a 90° excitation, let $\Delta S_{xy}(t) = M_{xyA}(t) - M_{xyB}(t)$ be the difference in transverse magnetization and $\Delta S_z(t) = M_{zA}(t) - M_{zB}(t)$ be the difference in longitudinal magnetization.
- (a) [5] Determine the time t that maximizes $|\Delta S_{xy}(t)|$.
- (b) [5] Determine the time t that maximizes $|\Delta S_z(t)|$.
- (c) [5] Evaluate your expressions for the case of 1T brain imaging of white matter ($T_1 = 680\text{ms}$, $T_2 = 92\text{ms}$), and gray matter ($T_1 = 820\text{ms}$, $T_2 = 100\text{ms}$).
- Assume the spins of interest in the two materials have the same resonant frequency and remain in phase.

MR imaging

3. [10] (a) [5] For the sinusoidally shaped k -space trajectory below, that starts at the origin, draw the timing diagram for the pulse sequence. Note that two excitations will be used to cover k -space; one for the top-half of k -space (where $k_y \geq 0$) and the other for the bottom half (where $k_y \leq 0$). Specify how the waveforms change between measurements.



- (b) [5] Determine the parameters (amplitudes and timing) of the gradient waveforms from part (a) that will approximately achieve $\text{FOV}_y = 19.2$ cm and $\Delta_x = \Delta_y = 0.3$ cm. (Do not worry about FOV_x .) Assume that Δ_y and FOV_y are based on the k -space coverage along the k_y axis. Also assume that the maximum gradient amplitude is 1 G/cm.
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4. [10] A 2D FT imaging sequence was designed using rectangular waveforms $G_y(t)$ of duration τ (and various amplitudes) for phase encoding. The design was based on the usual assumption that the induced field is linear, *i.e.*, $\vec{B}(r, t) = (B_{z0} + r \cdot G_y(t)) \hat{k}$. However, the actual field produced by the phase-encode gradient coil is nonlinear: $(y + \alpha y^3) G_y(t)$.
- (a) [5] Rewrite the signal equation for $s(t)$ in light of the nonlinearity in the y gradient.
- (b) [5] If the object is an impulse at (x_0, y_0) , *i.e.*, $m(x, y) = \delta_2(x - x_0, y - y_0)$, then determine at what position the impulse will be reconstructed by a usual reconstruction algorithm that is unaware of the gradient nonlinearity. (Such spatial distortions can be an important consideration when using MR for applications like surgical planning.)