Deep BCD-Net Using Identical Encoding-Decoding **ČNN** Structures for Iterative Image Recovery

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Abstract-In "extreme" computational imaging that collects extremely undersampled or noisy measurements, obtaining an accurate image within a reasonable computing time is challenging. Incorporating image mapping convolutional neural networks (CNN) into iterative image recovery has great potential to resolve this issue. This paper 1) incorporates image mapping CNN using identical convolutional kernels in both encoders and decoders into a block coordinate descent (BCD) signal recovery method and 2) applies alternating direction method of multipliers to train the aforementioned image mapping CNN. We refer to the proposed recurrent network as BCD-Net using identical encodingdecoding CNN structures. Numerical experiments show that, for a) denoising low signal-to-noise-ratio images and b) extremely undersampled magnetic resonance imaging, the proposed BCD-Net achieves significantly more accurate image recovery, compared to BCD-Net using distinct encoding-decoding structures and/or the conventional image recovery model using both wavelets and total variation.

I. INTRODUCTION

Using learned convolutional operators for iterative signal/image recovery is a growing trend in computational imaging [1]–[6], improving signal recovery performances over conventional non-trained regularizers (e.g., sparsity promoting regularizers) [4]–[6]. The iterative image recovery approaches that use learned convolutional operators or convolutional neural network (CNN) closely relate to challenging (nonconvex) block optimization. The authors in [4]-[6] proposed a fast and convergence-guaranteed block proximal gradient method using a majorizer to quickly and stably recover images with such image recovery approaches. Nonetheless, the corresponding iterative algorithm needs several hundreds of iterations to converge, detracting from its practical use.

By unfolding iterative signal recovery algorithms, there exist several works in combining neural network approaches into them [7]–[14]. By optimizing image mapping networks consisting of encoding and decoding kernels, thresholding operators, etc.-at each iteration (or layer), the methods moderate the aforementioned convergence issue, aiming to give "best" signal estimates at each layer. The authors in [14] incorporated iteration-wisely optimized image mapping networks into block coordinate descent (BCD) optimization method; referred to BCD-Net. However, encoding filters do not sufficiently capture rich information of training data (i.e., during training these

Algorithm I BCD-Net
Require: {Mapping⁽ⁱ⁾ :
$$i = 1, ..., N_{Nets}$$
}, $\mathbf{x}^{(0)}$, \mathbf{y} , $\lambda > 0$
for $i = 0, ..., N_{Nets} - 1$ do
 $\mathbf{z}^{(i+1)} = \text{Mapping}^{(i+1)}(\mathbf{x}^{(i)})$
 $\mathbf{x}^{(i+1)} = \underset{\mathbf{x} \in \mathbb{C}^{N}}{\operatorname{argmin}} f(\mathbf{x}; \mathbf{y}) + \lambda \|\mathbf{x} - \mathbf{z}^{(i+1)}\|_{2}^{2}$
end for

filters remain close to their initial conditions) [14], and this can limit the signal recovery performance of BCD-Net.

This paper 1) proposes a new BCD-Net using image mapping CNNs that use identical convolutional kernels in both encoders and decoders-we refer to this as the identical encoding-decoding CNN structure-and 2) applies alternating direction method of multipliers (ADMM [15]) to train the proposed BCD-Net. Numerical experiments show that, for a) denoising low signal-to-noise-ratio (SNR) images and b) extremely undersampled magnetic resonance imaging (MRI), the proposed BCD-Net significantly improves image recovery accuracy compared to BCD-Net using the distinct encodingdecoding structure [14] and/or the image recovery model using both wavelets and total variation (TV) (e.g., [16]).

II. BCD-NET FOR ITERATIVE SIGNAL RECOVERY: **IDENTICAL ENCODING-DECODING CNN STRUCTURE**

To recover a signal $\mathbf{x} \in \mathbb{C}^N$ from a measurement $\mathbf{y} \in \mathbb{C}^M$. we consider the following BCD optimization framework with two block variables x and z:

$$\underset{\mathbf{x}\in\mathbb{C}^{N}}{\operatorname{argmin}}\min_{\mathbf{z}\in\mathbb{C}^{N}} f(\mathbf{x};\mathbf{y}) + \lambda \|\mathbf{x} - \mathbf{z}\|_{2}^{2} + g(\mathbf{z}),$$
(1)

where $f(\mathbf{x}; \mathbf{y})$ is a data fitting term and $\mathbf{z} \in \mathbb{C}^N$ is a signal denoised by the regularizer $g(\mathbf{z})$. In imaging problems, $f(\mathbf{x}; \mathbf{y})$ relates to physical imaging models and noise statistics; e.g., a) for image denoising, $f(\mathbf{x}; \mathbf{y}) = \|\mathbf{y} - \mathbf{x}\|_2^2$ where \mathbf{y} is the noisy image corrupted by additive white Gaussian noise (AWGN); b) for MRI, $f(\mathbf{x}; \mathbf{y}) = \|\mathbf{y} - \mathbf{P}_{\Omega} \mathbf{F} \mathbf{x}\|_{2}^{2}$, where \mathbf{y} is the k-space measurement and $\mathbf{P}_{\Omega}\mathbf{F}$ is an undersampled Fourier operator with $\Omega \subseteq \{1, \ldots, N\}$. Examples of $g(\mathbf{z})$ include learned convolutional operators, e.g., convolutional dictionary [4], [5] and convolutional analysis operator [6]. The BCD-Net incorporates the iteration-wise trained image mapping networks into the BCD algorithmic framework in (1). See Algorithm 1.

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The signal recovery performance of BCD-Net largely depends on the performance of Mapping⁽ⁱ⁾($\mathbf{x}^{(i)}$) in Algorithm 1. Our goal is to reduce the number of layers by designing better image mapping networks that achieve more accurate image recovery. Motivated by designing $g(\mathbf{z})$ with the learned convolutional operators [4]–[6], we are particularly interested in the following image mapping CNN using the identical encoding-decoding structures:

$$\operatorname{Mapping}^{(i)}(\mathbf{x}^{(i)}) := \sum_{k=1}^{K} \mathbf{Sd}_{k}^{(i)} \circledast \mathcal{T}_{\alpha_{k}^{(i)}} \left(\left(\mathbf{d}_{k}^{(i)} \right)^{*} \circledast \mathbf{x}^{(i)} \right), \quad (P0)$$

for $i = 1, ..., N_{\text{Nets}}$, where $\operatorname{Mapping}^{(i)}(\cdot)$ denotes the trained mapping network at the *i*th layer and N_{Nets} is the number of layers in BCD-Net. Here, $\mathbf{d}_k^{(i)} \in \mathbb{C}^R$ denotes the *k*th filter at the *i*th layer, the soft thresholding operator $\mathcal{T}_{\mathbf{a}}(\mathbf{x}) : \mathbb{C}^N \to \mathbb{C}^N$ is defined by

$$(\mathcal{T}_{\mathbf{a}}(\mathbf{x}))_n := \begin{cases} x_n - a_n \cdot \operatorname{sign}(x_n), & |x_n| > a_n, \\ 0, & |x_n| \le a_n, \end{cases}$$
(2)

for $j = 1, \ldots, N$, sign (\cdot) is the (real or complex) sign function, and $\alpha_k^{(i)} \in \mathbb{R}$ denotes the *k*th thresholding value at the *i*th layer, $\mathbf{S} \in \mathbb{C}^{R \times R}$ flips a column vector in the vertical direction (e.g., it rotates 2D filters by 180°), *R* is the size of filters, *K* is the number of filters, and $(\cdot)^*$ indicates complex conjugate.

In the distinct encoding-decoding structure [14, (2)], the decoding filters evolved significantly during training while the encoding filters changed very little. In the proposed mapping structure (P0), we use same filters both in encoders and decoders to avoid this concern, i.e., we expect that (P0) can capture rich information of training data both in encoders and decoders—see Fig. 1 later.

III. TRAINING THE PROPOSED BCD-NET

Reformulating the convolutional operators in (P0) with a local approach (i.e., patch-based method) [6, §S.I], this section proposes an algorithm for training image mapping CNN (P0) in BCD-Net (see Algorithm 1). The training process requires L high-quality training images, { $\mathbf{x}_l^{\text{train}} : l = 1, ..., L$ }, and L training measurements simulated via imaging physics considered by $f(\mathbf{x}; \mathbf{y})$ in (1), { $\mathbf{y}_l^{\text{train}} : l = 1, ..., L$ }. At the *i*th layer, we train Mapping⁽ⁱ⁾ in (P0) as follows:

$$\left\{ \mathbf{D}^{(i)}, \boldsymbol{\alpha}^{(i)} \right\} = \underset{\{\mathbf{D}, \boldsymbol{\alpha}\}}{\operatorname{argmin}} \left\| \mathbf{X}_{\operatorname{train}}^{(i)} - \mathbf{D}\mathcal{T}_{\boldsymbol{\alpha}} \left(\mathbf{D}^{H} \mathbf{X}^{(i-1)} \right) \right\|_{F}^{2},$$

subj. to $\| \mathbf{d}_{k} \|_{2} \leq 1, \quad k = 1, \dots, K.$ (P1)

where $\mathbf{X}_{\text{train}}^{(i)}, \mathbf{X}^{(i-1)} \in \mathbb{C}^{R \times N'}$ are training data matrices in which columns correspond to N' patches randomly extracted from $\{\mathbf{x}_l^{\text{train}}\}$ and $\{\mathbf{x}_l^{(i-1)}\}$, respectively, $\{\mathbf{x}_l^{(i-1)} : l = 1, \ldots, L\}$ is a set of L images recovered at the (i-1)th layer, the filter matrix $\mathbf{D} \in \mathbb{C}^{R \times K}$ is defined by $\mathbf{D} := [\mathbf{d}_1, \cdots, \mathbf{d}_K]$, and $\boldsymbol{\alpha}^{(i)} \in \mathbb{R}^K$ is a vector consisting of K thresholding values. Algorithm 2 summarizes the training procedure.

To train Mapping⁽ⁱ⁾ via (P1), we update 2K blocks sequentially; at the kth block, we alternatively update the kth filter

Algorithm 2 Training BCD-Net
Require: {
$$\mathbf{x}_{l}^{\text{train}}, \mathbf{x}_{l}^{(0)}, \mathbf{y}_{l}^{\text{train}} : l = 1, ..., L$$
}, $\lambda > 0$
for $i = 0, ..., N_{\text{Nets}} - 1$ do
Train Mapping⁽ⁱ⁺¹⁾ (P0) via (P1) using { $\mathbf{x}_{l}^{\text{train}}, \mathbf{x}_{l}^{(i)}$ }
for $l = 1, ..., L$ do
 $\mathbf{z}_{l}^{(i+1)} = \text{Mapping}^{(i+1)}(\mathbf{x}_{l}^{(i)})$
 $\mathbf{x}_{l}^{(i+1)} = \underset{\mathbf{x}_{l} \in \mathbb{C}^{N}}{\operatorname{argmin}} f(\mathbf{x}_{l}; \mathbf{y}_{l}^{\text{train}}) + \lambda ||\mathbf{x}_{l} - \mathbf{z}_{l}^{(i+1)}||_{2}^{2}$
end for
end for

and thresholding value— $\mathbf{d}_{k}^{(i)}$ and $\alpha_{k}^{(i)}$, respectively. (P1) can be decomposed as $2K \{\mathbf{d}_{k}, \alpha_{k}\}$ -update problems [14]:

$$\left\{ \mathbf{d}_{k}^{(i)}, \alpha_{k}^{(i)} \right\} = \underset{\{\mathbf{d}_{k}, \alpha_{k}\}}{\operatorname{argmin}} \left\| \mathbf{E}_{k}^{(i)} - \mathbf{d}_{k} \mathcal{T}_{\alpha_{k}} \left(\mathbf{d}_{k}^{H} \mathbf{X}^{(i-1)} \right) \right\|_{F}^{2},$$

subj. to $\|\mathbf{d}_{k}\|_{2} \leq 1,$ (3)

where $\mathbf{E}_{k}^{(i)} := \mathbf{X}_{\text{train}}^{(i)} - \sum_{k' \neq k} \mathbf{d}_{k'} \mathcal{T}_{\alpha_{k'}} \left(\mathbf{d}_{k'}^{H} \widetilde{\mathbf{X}}^{(i)} \right)$. To solve (3), we alternatively update $\mathbf{d}_{k}^{(i)}$ and $\alpha_{k}^{(i)}$.

A. kth Thresholding Value Update

Using the current estimates of d_k , the *k*th thresholding value α_k is updated by subgradient descent method with backtracking line search (for step sizes) [14, §2].

B. kth Filter Update

Using the current update of α_k , we apply ADMM [15, §3.1.1] to update the *k*th filter \mathbf{d}_k . We update the *k*th filter \mathbf{d}_k by augmenting (3) with auxiliary variables (dropping the filter indices *k* and layer indices (i), (i - 1) for simplicity):

$$\mathbf{d}_{k} = \underset{\mathbf{d}}{\operatorname{argmin}} \left\| \mathbf{E} - \mathbf{d} \mathcal{T}_{\alpha}(\mathbf{v}^{H}) \right\|_{F}^{2}$$

subj. to $\|\mathbf{d}\|_{2} \leq 1$, $\mathbf{v} = \mathbf{X}^{H} \mathbf{d}$.

The cost function above has the corresponding augmented Lagrangian:

$$\begin{aligned} \mathcal{L}(\mathbf{d}, \mathbf{v}) &= \frac{1}{2} \left\| \mathbf{E} - \mathbf{d} \mathcal{T}_{\alpha}(\mathbf{v}^{H}) \right\|_{F}^{2} + \frac{\rho}{2} \left\| \mathbf{X}^{H} \mathbf{d} - \mathbf{v} + \mathbf{u} \right\|_{2}^{2} \\ &+ \mathcal{I}_{\{\mathbf{d}: \|\mathbf{d}\|_{2} \leq 1\}}(\mathbf{d}), \end{aligned}$$

where $\mathcal{I}_S(\mathbf{x})$ is the indicator function defined by $\mathcal{I}_S(\mathbf{x}) = 0$, if $\mathbf{x} \in S$, and $\mathcal{I}_S(\mathbf{x}) = \infty$, otherwise. We descend/ascend the augmented Lagrangian $\mathcal{L}(\mathbf{d}, \mathbf{v})$, using the following iterative updates of the primal, auxiliary, dual variables—**d**, **v**, and **u**, respectively:

$$\mathbf{v}^{(j+1)} = \underset{\mathbf{v}}{\operatorname{argmin}} \frac{1}{2} \left\| \mathbf{E} - \mathbf{d}^{(j)} \mathcal{T}_{\alpha}(\mathbf{v}) \right\|_{F}^{2} + \frac{\rho^{(j)}}{2} \left\| \mathbf{v} - \left(\mathbf{X}^{H} \mathbf{d}^{(j)} + \mathbf{u}^{(j)} \right) \right\|_{2}^{2}; \quad (4a)$$
$$\mathbf{d}^{(j+1)} = \underset{\mathbf{d}}{\operatorname{argmin}} \frac{1}{2} \left\| \mathbf{E} - \mathbf{d} \mathcal{T}_{\alpha} \left((\mathbf{v}^{(j+1)})^{H} \right) \right\|_{F}^{2} + \frac{\rho^{(j)}}{2} \left\| \mathbf{X}^{H} \mathbf{d} - \left(\mathbf{v}^{(j+1)} - \mathbf{u}^{(j)} \right) \right\|_{2}^{2}$$

$$+\mathcal{I}_{\{\mathbf{d}:\|\mathbf{d}\|_{2}=1\}}(\mathbf{d}); \tag{4b}$$

$$\mathbf{u}^{(j+1)} = \mathbf{u}^{(j)} + \mathbf{X}^H \mathbf{d}^{(j+1)} - \mathbf{v}^{(j+1)}, \qquad (4c)$$

where the ADMM parameters $\{\rho^{(j+1)}\}\$ are fixed or change based on some adaptive rules, e.g., residual balancing [15, §3.4.1].

We first consider problem (4b). Rewrite (4b) as follows:

$$\mathbf{d}^{(j+1)} = \underset{\mathbf{d}}{\operatorname{argmin}} \frac{\rho^{(j)}}{2} \mathbf{d}^{H} \mathbf{X} \mathbf{X}^{H} \mathbf{d} - \operatorname{Re} \left\{ \mathbf{d}^{H} \left(\mathbf{E} \mathcal{T}_{\alpha}(\mathbf{v}^{(j+1)}) + \rho^{(j)} \mathbf{X} \left(\mathbf{v}^{(j+1)} - \mathbf{u}^{(j)} \right) \right) \right\}$$

subj. to $\|\mathbf{d}\|_{2} \leq 1$, (5)

by $\|\mathbf{d}\mathcal{T}_{\alpha}(\mathbf{v}^{H})\|_{F}^{2} = c \cdot \|\mathcal{T}_{\alpha}(\mathbf{v})\|_{2}^{2}$ and $\operatorname{tr}(\mathcal{T}_{\alpha}(\mathbf{v}^{H})^{H}\mathbf{d}^{H}\mathbf{E}) = \mathbf{d}^{H}\mathbf{E}\mathcal{T}_{\alpha}(\mathbf{v})$, using $\mathcal{T}_{\alpha}(\mathbf{v}^{H})^{H} = \mathcal{T}_{\alpha}(\mathbf{v})$ and $\|\mathbf{d}\|_{2}^{2} = c \leq 1$. We apply an accelerated Newton's method to efficiently obtain the optimal solution to problem (5) [6, §IV-A3], [4, §IV-V-A2], considering that (5) is a (convex) quadratically constrained quadratic program. The closed form solution in [14, (4)] is not applicable for solving (4b), because of an additional quadratic term, e.g., the second term in (4b).

For problem (4a), we first rewrite (4a) as

$$\mathbf{v}^{(j+1)} = \underset{\mathbf{v}}{\operatorname{argmin}} \frac{1}{2} \left\| \mathcal{T}_{\alpha}(\mathbf{v}) - c^{-1} \cdot \mathbf{E}^{H} \mathbf{d}^{(j)} \right\|_{2}^{2} + \frac{\rho^{(j)}}{2c} \left\| \mathbf{v} - (\mathbf{X}^{H} \mathbf{d}^{(j)} + \mathbf{u}^{(j)}) \right\|_{2}^{2}$$
(6)

by applying the reformulation tricks used in (5). Using the separability of (6), we solve the following element-wise optimization problems:

$$v_n^{(j+1)} = \operatorname*{argmin}_{v_n} \frac{1}{2} \left| \mathcal{T}_\alpha(v_n) - g_n^{(j)} \right|^2 + \frac{\rho^{(j)}}{2c} \left| v_n - h_n^{(j)} \right|^2,$$
(7)

for n = 1, ..., N', where $\mathbf{g}^{(j)} := c^{-1} \mathbf{E}^H \mathbf{d}^{(j)}$ and $\mathbf{h}^{(j)} := \mathbf{X}^H \mathbf{d}^{(j)} + \mathbf{u}^{(j)}$. We solve (7) by subgradient descent method with backtracking line search: *a*) for the real-valued problem, we apply Lemma 1, and *b*) for the complex-valued problem, we apply Lemma 2.

Lemma 1. The gradient of $f(v) = \frac{1}{2}(\mathcal{T}_{\alpha}(v) - g)^2 + \frac{\rho}{2}(v - h)^2$ is given by

$$\partial f(v)/\partial v = (\mathcal{T}_{\alpha}(v) - g) \cdot 1_{|v| > \alpha} + \rho(v - h),$$

where $v, g, h \in \mathbb{R}$ and $\alpha, \rho > 0$.

Lemma 2. The gradient of $f(v) = \frac{1}{2}|\mathcal{T}_{\alpha}(v) - g|^2 + \frac{\rho}{2}|v - h|^2$ is given by

$$\frac{\partial f(v)}{\partial v} = (\mathcal{T}_{\alpha}(v) - g) \cdot \mathbf{1}_{|v| > \alpha} + \rho(v - h) \\ + i\alpha |v|^{-3} \cdot \operatorname{Im}\{v \cdot (\mathcal{T}_{\alpha}(v) - g)^*\} \cdot \mathbf{1}_{|v| > \alpha},$$

where $v, g, h \in \mathbb{C}$ and $\alpha, \rho > 0$. Distinct from the index *i*, we denote the imaginary unit by i.

Proof. See [17, Appx.].

Note that Lemma 1 is a special case of Lemma 2: when imaginary components of $\{v, g, h\}$ in Lemma 2 vanish, the gradient $\frac{\partial f(v)}{\partial v}$ in Lemma 2 becomes that in Lemma 1.



Fig. 1. Examples of trained filters for BCD-Net (MR image reconstruction; real components of complex-valued filters trained at the 10th layer). (a) Initial filters (discrete cosine transform). (b-c) Encoding and decoding filters trained by the image mapping module in [14]. (d) Filters trained with the proposed image mapping module using the identical encoding-decoding CNN structure.

IV. RESULTS AND DISCUSSION

A. Experimental Setup

1) Imaging and Image Recovery: For image denoising experiments, we contaminated five slices of XCAT phantom [18] by (zero-mean) AWGN with large standard deviation $\sigma \approx 135,202$ HU (that corresponds to $\sigma = 20,30$ for natural images within [0, 255]; we used four of them for training and the remaining one for testing. For MR image reconstruction experiments, we simulated two extremely undersampled (10%)k-space data sets with the optimal multi-level sampling in compressed sensing [19], [20] and field-of-view of 28×28cm on the 256×256 cartesian grid, while avoiding an inverse crime with two 768×768 complex-valued phantoms [21]; we used one for training and another for testing. We set the regularization parameter λ as follows: for image denoising, $\lambda = 10/\sigma'$, where σ' is scaled σ by considering the maximum value of XCAT phantom; for MR image reconstruction, $\lambda = 10^6$ (the same values were used for training BCD-Nets). We evaluated the quality of recovered images by peak SNR (PSNR).

2) Training BCD-Nets: We trained K = 64 filters of size $R = 8 \times 8$, with 20,000 randomly extracted image patches in each layer. For training BCD-Net using the distinct encodingdecoding CNN [14, (2)], we used the parameter set (including the number of subgradient descent iterations, filter initialization, initial thresholding values, etc.) in [14]. For training the proposed BCD-Net using the identical encoding-decoding CNN (P0), we used the parameter set in [14] as the default. The parameters related to ADMM in Section III-B are given as follows: we used 4 ADMM iterations and 4 inner subgradient descent iterations for updating $\mathbf{v}^{(j+1)}$ in (4a); and we applied the residual balancing scheme [15, §3.4.1] to adaptively control $\{\rho^{(j)}: \forall j \neq 0\}$ $(\rho^{(0)} = 1)$. We terminated the iterations of training each Mapping⁽ⁱ⁺¹⁾($\mathbf{x}^{(i)}$), if a) the relative difference stopping criterion (e.g., [4, (44)]) is met or b) the training costs (e.g., (P1)) increase, before reaching the maximum number of iterations. We set the relative difference tolerance as 2×10^{-3} ; and the maximum number of iterations to 120 and 180 for image denoising and MR image reconstruction, respectively.

B. Relation Between Filter Richness and Image Mapping Performance

The filters trained with the identical encoding-decoding CNN structure capture diverse features of training data. The rich features captured in filters are useful for better image



Fig. 2. Comparison of image denoising accuracy for different encoding-decoding structures in BCD-Net and noise levels (the cross mark x in (a) denotes a termination point). PSNR gaps between the two BCD-Nets are give as follows: (1) [0.58, 1.18]dB; (2) [0.92, 1, 32]dB; and (3) [0.16, 0.92]dB



Fig. 3. Comparison of reconstructed MR images from BCD-Nets using different image mapping CNN modules (at the 10th layer) and Sparse MRI reconstruction [16, built-in parameter setting]. (d) Compared to (b) (non-trained) Sparse MRI reconstruction, the proposed BCD-Net improves PSNR by 5dB.

mapping between corrupted and noiseless images, i.e., lower cost value in (P1). See Figs. 1–2(a). On the other hand, the filters trained with the distinct encoding-coding structure [14, (2)] do not sufficiently capture features of training data. See Fig. 1(b)–(c). (The result in Fig. 1(b) corresponds to that in [14, Fig. 2, transform rows].)

C. Application of Trained BCD-Nets to Iterative Image Denoising and MRI Image Reconstruction

Promoting better image mapping between the corrupted and noiseless images in training, the proposed BCD-Net (significantly) improves image recovery accuracy compare to the BCD-Net in [14]. PSNR gaps between the two BCD-Nets across the layers are given as follows: for denoising low SNR images ($\sigma = 30$), [0.92, 1.32]dB; for extremely undersampled MRI (10% sampling), [0.16, 0.92]dB. For the extremely undersampled MRI experiment, the PSNR gap increases as we increase the number of layers. See Fig. 2(b-3). Compared to the conventional MR reconstruction using wavelets and TV [16], the proposed BCD-Net significantly improves reconstruction accuracy only with 10 layers (or iterations): it improves PNSR by 5dB—see Fig. 3.

The drawback using BCD-Nets is that BCD-Nets are only applicable when the imaging models in training and testing are identical; meanwhile, the iterative signal recovery using learned CNNs is free from this limitation [4]–[6].

V. CONCLUSION

The proposed BCD-Net achieves accurate image recovery within a reasonable computing time in "extreme" computational imaging. The identical encoding-decoding CNN structure provides better image mapping than the distinct structure in [14, (2)], by better capturing rich information of training data. Future works include deriving closed-form solutions to (4a) for faster training of the proposed BCD-Net and testing its image mapping performances for more (locally) structured artifacts (e.g., aliasing artifacts caused by radial line or spiral undersampling in MRI, and streak artifacts caused by sparseview computed tomography).

REFERENCES

- M. D. Zeiler, D. Krishnan, G. W. Taylor, and R. Fergus, "Deconvolutional networks," in *Proc. IEEE CVPR*, San Francisco, CA, Jun. 2010, pp. 2528–2535.
- [2] F. Heide, W. Heidrich, and G. Wetzstein, "Fast and flexible convolutional sparse coding," in *Proc. IEEE CVPR*, Boston, MA, Jun. 2015, pp. 5135– 5143.
- [3] A. Serrano, F. Heide, D. Gutierrez, G. Wetzstein, and B. Masia, "Convolutional sparse coding for high dynamic range imaging," *Comput. Graph. Forum*, vol. 35, no. 2, pp. 153–163, May 2016.
 [4] I. Y. Chun and J. A. Fessler, "Convolutional dictionary learning: Accel-
- [4] I. Y. Chun and J. A. Fessler, "Convolutional dictionary learning: Acceleration and convergence," *IEEE Trans. Image Process.*, vol. 27, no. 4, pp. 1697–1712, Apr. 2018.
- [5] —, "Convergent convolutional dictionary learning using adaptive contrast enhancement (CDL-ACE): Application of CDL to image denoising," in *Proc. Sampling Theory and Appl. (SampTA)*, Tallinn, Estonia, Jul. 2017, pp. 460–464.
- [6] —, "Convolutional analysis operator learning: Acceleration, convergence, application, and neural networks," submitted, Jan. 2018.
- [7] K. Gregor and Y. LeCun, "Learning fast approximations of sparse coding," in *Proc. ICML*, Haifa, Israel, Jun, 2010, pp. 399–406.
- [8] Y. Yang, J. Sun, H. Li, and Z. Xu, "Deep ADMM-Net for compressive sensing MRI," in *Proc. NIPS* 29, Long Beach, CA, Dec. 2016, pp. 10– 18.
- [9] U. S. Kamilov and H. Mansour, "Learning optimal nonlinearities for iterative thresholding algorithms," *IEEE Signal Process. Lett.*, vol. 23, no. 5, pp. 747–751, Mar. 2016.
- [10] W. Zuo, D. Ren, D. Zhang, S. Gu, and L. Zhang, "Learning iterationwise generalized shrinkage-thresholding operators for blind deconvolution," *IEEE Trans. Image Process.*, vol. 25, no. 4, pp. 1751–1764, Feb. 2016.
- [11] Y. Chen and T. Pock, "Trainable nonlinear reaction diffusion: A flexible framework for fast and effective image restoration," *IEEE Trans. Pattern Anal. Mach. Intell.*, vol. 39, no. 6, pp. 1256–1272, Jun. 2017.
- [12] M. Borgerding, P. Schniter, and S. Rangan, "AMP-inspired deep networks for sparse linear inverse problems," *IEEE Trans. Signal Process.*, vol. 65, no. 16, pp. 4293–4308, Aug. 2017.
- [13] K. Hammernik, T. Klatzer, E. Kobler, M. P. Recht, D. K. Sodickson, T. Pock, and F. Knoll, "Learning a variational network for reconstruction of accelerated MRI data," *Magn. Reson. Med.*, Nov. 2017.
- [14] S. Ravishankar, I. Y. Chun, and J. A. Fessler, "Physics-driven deep training of dictionary-based algorithms for mr image reconstruction," in *Proc. Asilomar Conf. on Signals, Syst., and Comput.*, Pacific Grove, CA, Nov. 2017, pp. 1859–1863.
- [15] S. Boyd, N. Parikh, E. Chu, B. Peleato, and J. Eckstein, "Distributed optimization and statistical learning via the alternating direction method of multipliers," *Found. & Trends in Machine Learning*, vol. 3, no. 1, pp. 1–122, Jan. 2011.
- [16] M. Lustig, D. Donoho, and J. M. Pauly, "Sparse MRI: The application of compressed sensing for rapid MR imaging," *Magn. Reson. Med.*, vol. 58, no. 6, pp. 1182–1195, Dec. 2007.
- [17] I. Y. Chun and J. A. Fessler, "Deep BCD-net using identical encoding-decoding CNN structures for iterative image recovery," arXiv pre-print stat.ML/arXiv:1802.07129, Apr. 2018. [Online]. Available: https://arxiv.org/abs/1802.07129
- [18] W. P. Segars, M. Mahesh, T. J. Beck, E. C. Frey, and B. M. Tsui, "Realistic CT simulation using the 4D XCAT phantom," *Med. Phys.*, vol. 35, no. 8, pp. 3800–3808, Jul. 2008.
- [19] B. Adcock, A. C. Hansen, C. Poon, and B. Roman, "Breaking the coherence barrier: A new theory for compressed sensing," *Forum of Mathematics, Sigma 5*, 2017.
- [20] I. Y. Chun and B. Adcock, "Compressed sensing and parallel acquisition," *IEEE Trans. Inf. Theory*, vol. 63, no. 7, pp. 1–23, May 2017. [Online]. Available: http://arxiv.org/abs/1601.06214
- [21] M. Guerquin-Kern, L. Lejeune, K. P. Pruessmann, and M. Unser, "Realistic analytical phantoms for parallel Magnetic Resonance Imaging," *IEEE Trans. Med. Imag.*, vol. 31, no. 3, pp. 626–636, Mar. 2012.