

# Momentum optimization for iterative shrinkage algorithms in parallel MRI with sparsity-promoting regularization

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**Target Audience:** MR physicists and engineers working on accelerated imaging methods.

**Purpose:** Combinations of parallel MRI and compressed sensing have been proposed for reducing MRI scan time.<sup>1,2</sup> One can combine parallel MRI with compressed sensing by minimizing a cost function of the form,  $\Psi(x) = \frac{1}{2} \|y - Ax\|_2^2 + \beta \|Rx\|_1$ , where  $A$  is a SENSE system matrix and  $R$  is a sparsity-promoting transform (e.g., orthogonal wavelets). This cost function is difficult to minimize since the  $\ell_1$  term is nondifferentiable. Variable-splitting methods are one option for minimizing this function, but these require tuning of penalty parameters.<sup>2</sup> Majorize-minimize methods are an alternative that do not have these same penalty parameters, but they do require a tight bound for the behavior of  $RA'AR'$ .<sup>3</sup> BARISTA is an algorithm that gives a procedure for computing these bounds and combines it with momentum and adaptive momentum restarting.<sup>4</sup> Here, we review the BARISTA approach for orthogonal wavelets and propose a new momentum update that has a faster convergence rate. We also compare BARISTA to the AL-P2 algorithm,<sup>2</sup> a comparison that had not been made previously.

**Methods:** For brevity, we only describe the procedure for orthogonal wavelets. When the regularizer uses orthogonal wavelets we can instead optimize  $\tilde{\Psi}(z) = \frac{1}{2} \|y - AR'z\|_2^2 + \beta \|z\|_1$ , where  $x = R'z$ . Majorize-minimize methods require finding a surrogate function and then minimizing the surrogate. One such surrogate is to replace the quadratic term with  $\phi_k(z) = \frac{1}{2} \|z - (z^{(k)} - D_R^{-1}RA'(AR'z^{(k)} - y))\|_{D_R}^2$ , where  $z^{(k)}$  is the estimate of  $z$  at the  $k$ th iteration and  $D_R$  is a diagonal matrix such that  $D_R \geq RA'AR'$ . The minimum of  $\phi_k(z) + \beta \|z\|_1$  is calculated via the  $\ell_1$ -shrinkage operator. In Cartesian SENSE MRI,  $A'A \leq S'S$ , where  $S$  is a block-column matrix of sensitivity coil profiles. If  $R$  is an orthogonal wavelet transform, then we construct  $D_R$  by taking maximums over patches of the sum-of-squares of the sensitivity maps corresponding to the support size of the wavelet coefficient of interest.<sup>4,5</sup> To minimize  $\tilde{\Psi}(z)$  we iteratively apply shrinkage to  $\phi_k(z) + \beta \|z\|_1$  with  $D_R$  constructed in this manner. This approach extends to analysis regularizers such as total variation.<sup>4</sup> Accelerating the method with momentum<sup>3</sup> and adaptive restarting<sup>6</sup> gives BARISTA.<sup>4</sup> We propose to further accelerate BARISTA by using a new momentum update:  $u^{(k+1)} = z^{(k+1)} + \frac{\tau^{(k)} - 1}{\tau^{(k+1)}} (z^{(k+1)} - z^{(k)}) + \frac{\tau^{(k)}}{\tau^{(k+1)}} (z^{(k+1)} - u^{(k)})$ , which gives a theoretical factor of 2 increase in convergence speed of the cost function.<sup>7</sup> We applied BARISTA with this new momentum term and compared convergence speed to previous methods. Our experiments consisted of collecting a 144 by 256 by 128 sample 3D data set on a GE 3T scanner with an 8-channel head coil. One slice was selected for experiments. The data were retrospectively downsampled with a Poisson-disk sampling pattern with a densely-sampled center. We then minimized  $\Psi(x)$  with BARISTA, split Bregman (with optimized parameters for this data set, denoted SB), AL-P2 with parameters based on heuristics (denoted AL-P2),<sup>2</sup> AL-P2 with optimized parameters (denoted AL-P2, opt), and our proposed optimized momentum BARISTA (OMBARISTA) to compare convergence speed.

**Results:** We plot  $\xi(k) = \frac{\|x^{(k)} - x^{(\infty)}\|}{\|x^{(\infty)}\|}$ , the norm-residual to convergence, vs. time in all figures.  $x^{(\infty)}$  was calculated by running many thousands of iterations. Figure 2 compares the convergence speed of the algorithms in the orthogonal Haar wavelet case, showing the  $\sqrt{2}$ -factor increase in norm-residual convergence speed. Figure 3 compares the convergence speed with undecimated Haar wavelets. The difference is not as large as with the orthogonal Haar case since the undecimated Haar algorithm requires solving a denoising subproblem,<sup>4</sup> but OMBARISTA is still the fastest method.

**Discussion:** In addition to converging rapidly, the methods presented use parameters that are easier to tune than the penalty parameters used by variable-splitting methods, making them more robust to use in a clinical setting. We also observed the theoretically-predicted increase in convergence speed with the new momentum term. In conclusion, we have made an improvement to a fast algorithm and observed faster convergence with the new algorithm than current state-of-the-art methods.

**References:** 1. Lustig et. al, MRM 2007, 2. Ramani et. al, IEEE-TMI 2011, 3. Beck et. al, SIAM-JIS 2009, 4. Muckley et. al, IEEE-TMI to appear, 5. Muckley et. al, ICIP 2014, 6. O'Donoghue et. al, FCM, 7. Kim et. al, arXiv 2014.

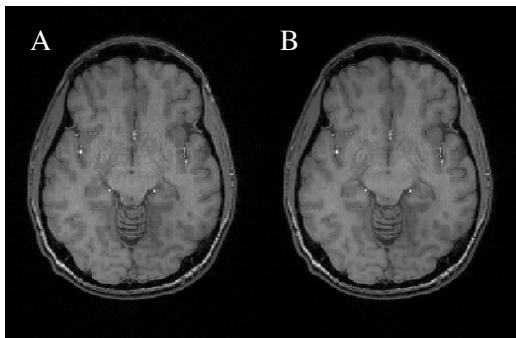


Figure 1: A) Image estimated with orthogonal Haar wavelets. B) Image estimated by minimizing  $\Psi(x)$  with 2-level undecimated Haar wavelets

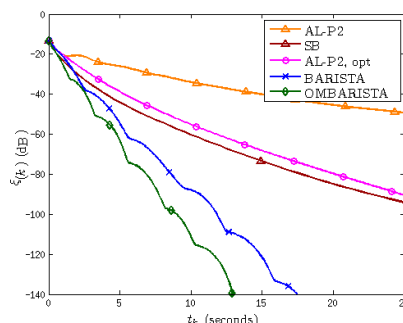


Figure 2: Convergence plot using orthogonal Haar regularizer, showing  $\sqrt{2}$  increase in  $\Psi(x)$  with 2-level undecimated Haar wavelets. speed.

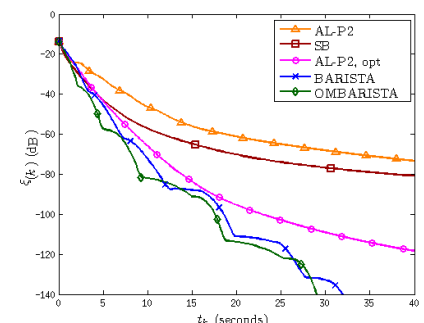


Figure 3: Convergence plot for minimizing  $\Psi(x)$  with 2-level undecimated Haar wavelets. AL-P2 requires parameter optimization for this data set to have comparable speed.